

Package ‘AnalyzefMRI’

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Title Functions for analysis of fMRI datasets stored in the ANALYZE or NIFTI format.

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Depends tcltk, R.matlab, fastICA

Description Functions for I/O, visualisation and analysis of functional Magnetic Resonance Imaging (fMRI) datasets stored in the ANALYZE or NIFTI format.

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analyze2nifti	<i>Create a NIFTI file from an Analyze file</i>
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Description

Create a NIFTI file from an Analyze file.

Usage

```
analyze2nifti(file.in,path.in=".",path.out=".",file.out=NULL,is.nii=TRUE,qform.code
```

Arguments

<code>file.in</code>	character, filename of the Analyze file to be read
<code>path.in</code>	character, Directory path from where to take the .hdr,.img,.mat files
<code>path.out</code>	character, Directory path where to write the .hdr/.img or .nii file
<code>file.out</code>	character, filename of the NIFTI file to write (without extension). If NULL, same as <code>file.in</code>
<code>is.nii</code>	logical, if TRUE a NIFTI .nii file will be created, if FALSE a .hdr/.img NIFTI file will be created
<code>qform.code</code>	qform.code value (in 0,...4)

<code>sform.code</code>	sform.code value (in 0,...4)
<code>data.type</code>	char[10]. UNUSED in NIFTI-1 but could be filled with what you want
<code>db.name</code>	char[18]. UNUSED in NIFTI-1 but could be filled with what you want
<code>dim.info</code>	MRI slice ordering: This field encode which spatial dimension (1=x, 2=y, or 3=z) corresponds to which acquisition dimension for MRI data. In fact, it contains three informations: <code>freq.dim</code> , <code>phase.dim</code> and <code>slice.dim</code> , all squished into the single byte field <code>dim.info</code> (2 bits each, since the values for each field are limited to the range 0..3). The R function <code>fps2diminfo</code> can be used to encode these values from the <code>dim.info</code> byte.
<code>dim</code>	vector (of length 8) of image dimensions. <code>dim[1]</code> specifies the number of dimensions. In NIFTI-1 files, <code>dim[2]</code> , <code>dim[3]</code> , <code>dim[4]</code> are for space, <code>dim[5]</code> is for time. The 5th dimension (<code>dim[6]</code>) of the dataset, if present (i.e., <code>dim[1]=5</code> and <code>dim[6] > 1</code>), contains multiple values (for example a vector) to be stored at each spatiotemporal location. Uses of <code>dim[7]</code> and <code>dim[8]</code> are not specified in NIFTI-1 format.
TR	Time Repetition to be stored in <code>pixdim[5]</code>
<code>slice.code</code>	Slice timing order. If this is nonzero, AND if <code>slice.dim</code> is nonzero, AND if <code>slice.duration</code> is positive, indicates the timing pattern of the slice acquisition. The following codes are defined: 0 (NIFTI SLICE UNKNOWN), 1 (NIFTI SLICE SEQ INC), 2 (NIFTI SLICE SEQ DEC), 3 (NIFTI SLICE ALT INC), 4 (NIFTI SLICE ALT DEC)
<code>xyzt.units</code>	Units of <code>pixdim[2:5]</code> . Bits 1..3 of <code>xyzt.units</code> specify the (same) space unit of <code>pixdim[2:4]</code> . Bits 4..6 of <code>xyzt.units</code> specify the time unit of <code>pixdim[5]</code> . See <code>xyzt-units.txt</code> in the <code>niftidoc</code> directory of the source package. The R function <code>st2xyzt</code> can be used to encode these values from the <code>xyzt.units</code> byte.
<code>descrip</code>	char[80]. This field may contain any text you like
<code>aux.file</code>	char[24]. This field is used to store an auxiliary filename.
<code>intent.name</code>	char[16]. 'name' or meaning of data. If no data name is implied or needed, <code>intent.name[1]</code> should be set to 0.

Value

Nothing is returned. The NIFTI file is created in the specified `path.out` directory (default is current directory).

Examples

```
analyze2nifti(path.in=system.file(package="AnalyzefMRI"), file.in="example", file.out="nifti-t
```

centering *centering*

Description

This function center the data in the two dimensions, the first dimension being indicated by col.first argument

Usage

```
centering(X, col.first=TRUE)
```

Arguments

X a matrix of size tm x vm which contains the fonctionnal images
col.first Logical. Center the columns or the rows first

Value

Xcentred the double centered matrix

See Also

[reduction](#)

Examples

```
# TODO!!  
# Xcentred <- centering(X.masked,col.first=TRUE)$Xcentred
```

cluster.threshold *Cluster threshold an array.*

Description

Calculate contiguous clusters of locations in a 3D array that are above some threshold and with some minimum size.

Usage

```
cluster.threshold(x, nmat = NULL, level.thr = 0.5, size.thr)
```

Arguments

<code>x</code>	A 3D array
<code>nmat</code>	A matrix with 3 columns specifying the neighbourhood system. Default is 6 nearest neighbours in 3D.
<code>level.thr</code>	The level at which to threshold the array values. Default is 0.5 and is designed to cluster 0-1 arrays.
<code>size.thr</code>	The cluster size threshold.

Value

Returns an array of the same size as `x` with a 1 at all locations which have a value above `level.thr` and are in a cluster of similar locations with size greater than `size.thr`.

Author(s)

J. L. Marchini

Examples

```
x <- array(0, dim = c(64, 64, 21))
x[10:20, 10:20, 1:5] <- 1
x[30:40, 30:40, 6:7] <- 1
x[50, 50, 8:9] <- 1

a <- cluster.threshold(x, size.thr = 400)
sum(x) ## should be 849
sum(a) ## should be 605
```

`cov.est`

Estimates the covariance between neighbouring voxels

Description

Estimates the covariance between neighbouring voxels using a specified neighbourhood system.

Usage

```
cov.est(mat, mask, nmat)
```

Arguments

<code>mat</code>	3D array of voxel values.
<code>mask</code>	Array with same dimension as <code>mat</code> that is 1/0 for voxels to be included/excluded.
<code>nmat</code>	Neighbourhood matrix.

Value

The estimated covariance

Author(s)

J. L. Marchini

Examples

```
ksize <- 9
d <- c(64, 64, 21)
FWHM <- 9
sigma <- diag(FWHM^2, 3) / (8 * log(2))
voxdim <- c(2, 2, 4)

filtermat <- GaussSmoothKernel(voxdim, ksize, sigma)

mask <- array(1, dim = d)
num.vox <- sum(mask)

mat <- Sim.3D.GRF(d = d, voxdim = voxdim, sigma = sigma, ksize = ksize, mask = mask, type =

nmat <- expand.grid(-1:1, -1:1, -1:1)
nmat4 <- nmat[c(11, 13, 15, 17), ]

cov <- cov.est(mat, mask, nmat4)
```

diminfo2fps

diminfo2fps

Description

Extract freq.dim, phase.dim and slice.dim fields from the one byte dim.info field of a NIFTI header file.

Usage

```
diminfo2fps(dim.info)
```

Arguments

`dim.info` dim.info field of a NIFTI header file

Value

A list containing freq.dim, phase.dim and slice.dim fields.

See Also

[fps2diminfo](#)

Examples

```
dim.info <- f.read.header(system.file("example-nifti.hdr", package="AnalyzeFMRI"))$dim.info
diminfo2fps(dim.info)
```

 EC.3D

Expected Euler Characteristic for a 3D Random Field

Description

Calculates the Expected Euler Characteristic for a 3D Random Field thresholded at a level u .

Usage

```
EC.3D(u, sigma, voxdim = c(1, 1, 1), num.vox, type = c("Normal", "t"), df = NULL)
```

Arguments

<code>u</code>	The threshold for the field.
<code>sigma</code>	The spatial covariance matrix of the field.
<code>voxdim</code>	The dimensions of the cuboid 'voxels' upon which the discretized field is observed.
<code>num.vox</code>	The number of voxels that make up the field.
<code>type</code>	The marginal distribution of the Random Field (only Normal and t at present).
<code>df</code>	The degrees of freedom of the t field.

Details

The Euler Characteristic χ_u (Adler, 1981) is a topological measure that essentially counts the number of isolated regions of the random field above the threshold u minus the number of 'holes'. As u increases the holes disappear and χ_u counts the number of local maxima. So when u becomes close to the maximum of the random field Z_{\max} we have that

$$P(\text{reject } H_0 | H_0 \text{ true}) = P(Z_{\max}) = P(\chi_u > 0) \approx E(\chi_u)$$

where H_0 is the null hypothesis that there is no significant positive activation/signal present in the field. Thus the Type I error of the test can be controlled through knowledge of the Expected Euler characteristic.

Value

The value of the expected Euler Characteristic.

Author(s)

J. L. Marchini

References

Adler, R. (1981) *The Geometry of Random Fields*. New York: Wiley. Worlsey, K. J. (1994) Local maxima and the expected euler characteristic of excursion sets of χ^2 , f and t fields. *Advances in Applied Probability*, **26**, 13-42.

See Also[Threshold.RF](#)**Examples**

```
EC.3D(4.6, sigma = diag(1, 3), voxdim = c(1, 1, 1), num.vox = 10000)
```

```
EC.3D(4.6, sigma = diag(1, 3), voxdim = c(1, 1, 1), num.vox = 10000, type = "t", df = 100)
```

eigenvalues

eigenvalues

Description

This function computes the eigenvalues of a centered and reduced data matrix

Usage

```
eigenvalues(X, draw=FALSE)
```

Arguments

`X` a matrix of size $t_m \times v_m$ which contains the functional images centered and reduced

`draw` Logical. Should we plot the eigenvalues

Value

A list containing

`eigenvalues` vector of the eigenvalues

Examples

```
# TODO!!
# valpcr <- eigenvalues(Xcr, draw=T)$eigenvalues
```

```
f.analyze.file.summary  
prints summary of .img file contents
```

Description

Prints a summary of the contents of an ANALYZE .img file using the associated .hdr header file.

Usage

```
f.analyze.file.summary(file)
```

Arguments

file The location of .img file to be read

Value

A print out containing information about the .img file. This includes File name, Data Dimension, X dimension, Y dimension, Z dimension, Time dimension, Voxel dimensions, Data type

See Also

```
f.read.analyze.header, f.read.analyze.slice, f.read.analyze.slice.at.all.timepoints,  
f.read.analyze.ts, f.write.analyze, f.read.analyze.volume, f.spectral.summary,  
f.write.array.to.img.2bytes, f.write.array.to.img.float, f.write.list.to.hdr,  
f.basic.hdr.list.create
```

Examples

```
f.analyze.file.summary(system.file("example.img", package="AnalyzeFMRI"))
```

```
f.analyzeFMRI.gui    starts AnalyzeFMRI GUI
```

Description

Starts an R/tk interfaced GUI that allows the user to explore an fMRI dataset stored in an ANALYZE format file using the functions of the AnalyzeFMRI package.

Usage

```
f.analyzeFMRI.gui()
```

Value

No value is returned

```
f.basic.hdr.list.create
      creates basic .hdr list in ANALYZE format
```

Description

Creates a basic list that can be used to write a .hdr file

Usage

```
f.basic.hdr.list.create(mat, file.hdr)
```

Arguments

mat	mat Array that is to be converted to a .img file
file.hdr	file.hdr Name of the .hdr file that will be created

Value

Returns a list of all the fields needed to create a .hdr file (see the functions code for details).

See Also

[f.write.list.to.hdr](#), [f.analyze.file.summary](#)

Examples

```
a<-array(rnorm(20*30*40*3),dim=c(20,30,40,3))
file<-"temp.hdr"
f.basic.hdr.list.create(a, file)
```

```
f.basic.hdr.nifti.list.create
      creates basic .hdr list in NIFTI format
```

Description

Creates a basic list that can be used to write a .hdr file or the header part of a .nii file

Usage

```
f.basic.hdr.nifti.list.create(dim.mat, file)
```

Arguments

<code>dim.mat</code>	<code>dim.mat</code> vector of the dimensions of the image array associated with the header file to be written
<code>file</code>	<code>file</code> Name of the .hdr file that will be contained in the file field of the header

Value

Returns a list of all the fields needed to create a .hdr file (see the function code for details).

See Also

[f.write.list.to.hdr.nifti](#), [f.nifti.file.summary](#)

Examples

```
dim.mat <- c(20,30,40,3)
file<-"temp.hdr"
f.basic.hdr.nifti.list.create(dim.mat, file)
```

```
f.complete.hdr.nifti.list.create
      creates complete .hdr list in NIFTI format
```

Description

Creates a complete list that can be used to write a .hdr file or the header part of a .nii file

Usage

```
f.complete.hdr.nifti.list.create(file,dim.info=character(1),dim,intent.pl=single(1))
```

Arguments

<code>file</code>	The .hdr filename. If file extension is ".nii", this will create a header file for a ".nii" NIFTI file, else for a .hdr/.img NIFTI pair
<code>dim.info</code>	MRI slice ordering: This field encode which spatial dimension (1=x, 2=y, or 3=z) corresponds to which acquisition dimension for MRI data. In fact, it contains three informations: freq.dim, phase.dim and slice.dim, all squished into the single byte field dim.info (2 bits each, since the values for each field are limited to the range 0..3). The R function <code>fps2diminfo</code> can be used to encode these values into the dim.info character byte.
<code>dim</code>	vector (of length 8) of image dimensions. <code>dim[1]</code> specifies the number of dimensions. In NIFTI-1 files, <code>dim[2]</code> , <code>dim[3]</code> , <code>dim[4]</code> are for space, <code>dim[5]</code> is for time. The 5th dimension (<code>dim[6]</code>) of the dataset, if present (i.e., <code>dim[1]=5</code> and <code>dim[6] > 1</code>), contains multiple values (for example a vector) to be stored at each spatio-temporal location. Uses of <code>dim[7]</code> and <code>dim[8]</code> are not specified in NIFTI-1 format.

<code>intent.p1</code>	1st intent parameter: first auxiliary parameter for a possible statistical distribution specified in <code>intent.code</code>
<code>intent.p2</code>	2nd intent parameter: second auxiliary parameter for a possible statistical distribution specified in <code>intent.code</code>
<code>intent.p3</code>	3rd intent parameter: third auxiliary parameter for a possible statistical distribution specified in <code>intent.code</code>
<code>intent.code</code>	NIFTI INTENT code: if 0, this is a raw dataset; if in range 2...24, this indicates that the numbers in the dataset should be interpreted as being drawn from a given distribution. Most such distributions have auxiliary parameters (given with <code>intent.p?</code>); if in range 1001...1011, this is an other meaning. See file <code>intent-code.txt</code> in the <code>niftidoc</code> directory of the source package. If the dataset DOES NOT have a 5th dimension (<code>dim[1]=4</code>), then the auxiliary parameters are the same for each voxel, and are given in header fields <code>intent.p1</code> , <code>intent.p2</code> , and <code>intent.p3</code> . If the dataset DOES have a 5th dimension (<code>dim[1]=5</code>), then the auxiliary parameters are different for each voxel.
<code>datatype</code>	integer indicator of data storage type for each voxel. This could be 2 (unsigned char), 4 (signed short), 8 (signed int), 16 (32 bit float), 32 (64 bit complex = two 32 bit floats), 64 (64 bit float = double), 128 (3 8 bit bytes), 256 (signed char), 512 (unsigned short), 768 (unsigned int), 1024 (signed long long), 1280 (unsigned long long), 1536 (128 bit float = long double), 1792 (128 bit complex = 2 64 bit floats), 2048 (256 bit complex = 2 128 bit floats).
<code>bitpix</code>	the number of bits per voxel. This field MUST correspond with the <code>datatype</code> field. The total number of bytes in the image data is $\text{dim}[2] * \dots * \text{dim}[\text{dim}[1]+1] * \text{bitpix} / 8$
<code>slice.start</code>	Indicates the start of the slice acquisition pattern, when <code>slice.code</code> is nonzero. These values are present to allow for the possible addition of "padded" slices at either end of the volume, which don't fit into the slice timing pattern. If there are no padding slices, then <code>slice.start=0</code> and <code>slice.end=dim[slice.dim+1]-1</code> are the correct values. For these values to be meaningful, <code>slice.start</code> must be non-negative and <code>slice.end</code> must be greater than <code>slice.start</code> .
<code>pixdim</code>	vector (of length 8). Grid spacings. When reading a NIFTI-1 header, <code>pixdim[1]</code> stores <code>qfac</code> (which is either -1 or 1). If <code>pixdim[1]=0</code> (which should not occur), we take <code>qfac=1</code> . <code>pixdim[2]</code> , <code>pixdim[3]</code> and <code>pixdim[4]</code> give the voxel width along dimension x, y and z respectively. <code>pixdim[5]</code> gives the time step (=Time Repetition=TR). The units of <code>pixdim</code> can be specified with the <code>xyzt.units</code> field.
<code>scl.slope</code>	Data scaling: If the <code>scl.slope</code> field is nonzero, then each voxel value in the dataset should be scaled as $y = \text{scl.slope} * x + \text{scl.inter}$, where x = voxel value stored and y = "true" voxel value
<code>scl.inter</code>	Data scaling: offset. Idem above.
<code>slice.end</code>	Indicates the end of the slice acquisition pattern, when <code>slice.code</code> is nonzero. These values are present to allow for the possible addition of "padded" slices at either end of the volume, which don't fit into the slice timing pattern. If there are no padding slices, then <code>slice.start=0</code> and <code>slice.end=dim[slice.dim+1]-1</code> are the correct values. For these values to be meaningful, <code>slice.start</code> must be non-negative and <code>slice.end</code> must be greater than <code>slice.start</code> .

<code>slice.code</code>	Slice timing order. If this is nonzero, AND if <code>slice.dim</code> is nonzero, AND if <code>slice.duration</code> is positive, indicates the timing pattern of the slice acquisition. The following codes are defined: 0 (NIFTI SLICE UNKNOWN), 1 (NIFTI SLICE SEQ INC), 2 (NIFTI SLICE SEQ DEC), 3 (NIFTI SLICE ALT INC), 4 (NIFTI SLICE ALT DEC)
<code>xyzt.units</code>	Units of <code>pixdim[2:5]</code> . Bits 1..3 of <code>xyzt.units</code> specify the (same) space unit of <code>pixdim[2:4]</code> . Bits 4..6 of <code>xyzt.units</code> specify the time unit of <code>pixdim[5]</code> . See <code>xyzt-units.txt</code> in the <code>niftidoc</code> directory of the source package. The R function <code>st2xyzt</code> can be used to encode these values into the <code>xyzt.units</code> byte.
<code>cal.max</code>	Maximum display intensity (white) corresponds to dataset value <code>cal.max</code> . Dataset values above <code>cal.max</code> should display as white. <code>cal.min</code> and <code>cal.max</code> only make sense when applied to scalar-valued datasets (i.e., <code>dim[1] < 5</code> or <code>dim[6] = 1</code>).
<code>cal.min</code>	Minimum display intensity (black) corresponds to dataset value <code>cal.min</code> . Dataset values below <code>cal.min</code> should display as black.
<code>slice.duration</code>	Time for 1 slice. If this is positive, AND if <code>slice.dim</code> is nonzero, indicates the amount of time used to acquire 1 slice.
<code>toffset</code>	Time axis shift: The <code>toffset</code> field can be used to indicate a nonzero start point for the time axis. That is, time point <code>m</code> is at <code>t=toffset+m*pixdim[5]</code> for <code>m=1, ..., dim[5]-1</code> .
<code>descrip</code>	<code>char[80]</code> . This field may contain any text you like
<code>aux.file</code>	<code>char[24]</code> . This field is used to store an auxiliary filename.
<code>qform.code</code>	NIFTI code (in 0, ... ,4). 0: Arbitrary coordinates; 1: Scanner-based anatomical coordinates; 2: Coordinates aligned to another file's, or to anatomical "truth" (coregistration); 3: Coordinates aligned to Talairach-Tournoux Atlas; 4: MNI 152 normalized coordinates
<code>sform.code</code>	NIFTI code (in 0, ... ,4) with the same meaning as <code>qform</code> codes. The basic idea behind having two coordinate systems is to allow the image to store information about (1) the scanner coordinate system used in the acquisition of the volume (in the <code>qform</code>) and (2) the relationship to a standard coordinate system - e.g. MNI coordinates (in the <code>sform</code>). The <code>qform</code> allows orientation information to be kept for alignment purposes without losing volumetric information, since the <code>qform</code> only stores a rigid-body transformation (rotation and translation) which preserves volume. On the other hand, the <code>sform</code> stores a general affine transformation (shear, scale, rotation and translation) which can map the image coordinates into a standard coordinate system, like Talairach or MNI, without the need to resample the image. By having both coordinate systems, it is possible to keep the original data (without resampling), along with information on how it was acquired (<code>qform</code>) and how it relates to other images via a standard space (<code>sform</code>). This ability is advantageous for many analysis pipelines, and has previously required storing additional files along with the image files. By using NIfTI-1 this extra information can be kept in the image files themselves. Note: the <code>qform</code> and <code>sform</code> also store information on whether the coordinate system is left-handed or right-handed and so when both are set they must be consistent, otherwise the handedness of the coordinate system (often used to distinguish left-right order) is unknown and the results of applying operations to such an image are unspecified.

quatern.b	Quaternion b param. These b,c,d quaternion parameters encode a rotation matrix used when qform.code > 0 to obtain a rigid transformation that maps voxel indices (i,j,k) to spatial coordinates (x,y,z), typically anatomical coordinates assigned by the scanner. This transformation ("Method 2" in the nifti1.h documentation) is generated using also the voxel dimensions (pixdim[1:4]) and a 3D shift, i.e. a translation, (qoffset.*)
quatern.c	Quaternion c param
quatern.d	Quaternion d param
qoffset.x	Quaternion x shift. If the (0020,0032) DICOM attribute is extracted into (px,py,pz), then qoffset.x = -px qoffset.y = -py qoffset.z = pz is a reasonable setting when qform.code=NIFTI XFORM SCANNER ANAT.
qoffset.y	Quaternion y shift
qoffset.z	Quaternion z shift
srow.x	vector of length 4. 1st row affine transform. These srow.* parameters contain an affine (non-rigid) transformation ("Method 3" in the nifti1.h documentation) that maps voxel indices (i,j,k) to spatial coordinates (x,y,z).
srow.y	vector of length 4. 2nd row affine transform
srow.z	vector of length 4. 3rd row affine transform
intent.name	char[16]. 'name' or meaning of data. If no data name is implied or needed, intent.name[1] should be set to 0.

Value

Returns a list of all the fields needed to create a .hdr file (see the function code for details).

See Also

[f.basic.hdr.nifti.list.create](#), [f.write.list.to.hdr.nifti](#), [f.nifti.file.summary](#)

Examples

```
dim.mat <- c(20,30,40,3)
dim <- c(length(dim.mat), dim.mat, rep(0, 7 - length(dim.mat)))
filename <- "temp.hdr"
f.complete.hdr.nifti.list.create(file=filename,dim=dim)
```

f.ica.fmri

Applies Spatial ICA (Independent Component Analysis) to fMRI datasets

Description

Decomposes an fMRI dataset into a specified number of Spatially Independent Components maps and associated time-courses using the FastICA algorithm

Usage

```
f.ica.fmri(file.name, n.comp, norm.col=TRUE, fun="logcosh", maxit=1000,
alg.type="parallel", alpha=1, tol=1e-04, mask.file.name=NULL, slices=NULL)
```

Arguments

file.name	path to fMRI dataset (ANALYZE format .img file)
n.comp	number of components to extract
norm.col	a logical value indicating whether each voxel time series should be standardised to have zero mean and unit variance before the ICA algorithm is applied (default=TRUE recommended in practice)
fun	the functional form of the G function used in the approximation to negentropy (see details)
maxit	maximum number of iterations to perform
alg.type	if alg.type=="deflation" the components are extracted one at a time (the default). if alg.type=="parallel" the components are extracted simultaneously.
alpha	constant in range [1,2] used in approximation to negentropy when fun=="logcosh"
tol	a positive scalar giving the tolerance at which the un-mixing matrix is considered to have converged.
mask.file.name	Optional path to file containing a 0/1 mask for the dataset
slices	Optional vector of slices to be included

Details

The fMRI dataset is rearranged into a 2-dimensional data matrix X , where the column vectors are voxel time-series. A mask is used to specify which voxels are included. If this is not supplied by the user then a mask is constructed automatically using a 10% intensity threshold.

The data matrix is considered to be a linear combination of non-Gaussian (independent) components i.e. $X = AS$ where rows of S contain the independent components and A is a linear mixing matrix. In short ICA attempts to 'un-mix' the data by estimating an un-mixing matrix U where $UX = S$.

Under this generative model the measured 'signals' in X will tend to be 'more Gaussian' than the source components (in S) due to the Central Limit Theorem. Thus, in order to extract the independent components/sources we search for an un-mixing matrix U that maximizes the non-gaussianity of the sources.

In FastICA, non-gaussianity is measured using approximations to negentropy (J) which are more robust than kurtosis based measures and fast to compute.

The approximation takes the form

$$J(y) = [EG(y) - EG(v)]^2 \text{ where } v \text{ is a } N(0,1) \text{ r.v}$$

The following choices of G are included as options $G(u) = \frac{1}{\alpha} \log \cosh(\alpha u)$ and $G(u) = -\exp(\frac{-u^2}{2})$

The FastICA algorithm is used to 'un-mix' the data and recover estimates of the mixing matrix A and the source matrix S . Rows of the source matrix S represent spatially independent components

of the dataset (these are arranged spatially in the output). Columns of A contain the associated time-courses of the independent components.

Pre-processing involves removing the mean of each row of the data matrix and (optionally) standardizing the columns of the data matrix to have zero mean and unit variance.

All computations are done using C code. This avoids reading the entire dataset into R and thus saves memory space.

Value

A list containing the following components

A	estimated mixing matrix
S	estimated source matrix that has been rearranged spatially i.e. S is a 4-D array and S[,,i] contains the 3-D map of the ith component
file	the name of the data file
mask	the name of the mask file

Author(s)

J L Marchini <marchini@stats.ox.ac.uk> and C Heaton <chrisheaton99@yahoo.com>

References

A. Hyvarinen and E. Oja (2000) Independent Component Analysis: Algorithms and Applications, Neural Networks, 13(4-5):411-430

Beckmann C. (2000) Independent Component Analysis for fMRI. First Year D.Phil Report, Dept. of Engineering Science, University of Oxford.

See Also

[f.ica.fmri.gui](#), [f.plot.ica.fmri](#)

f.ica.fmri.gui *tcltk GUI to apply ICA to fMRI datasets*

Description

The GUI provides a quick and easy to use interface for applying spatial ICA to fMRI datasets. Computations are done in C for speed and low memory usage.

Usage

```
f.ica.fmri.gui()
```

Details

The user is required to enter the location of the fMRI dataset (stored in the ANALYZE format) and (optionally) a mask for the dataset. If no mask is supplied then an option to create mask is available. There is option to normalize the columns of the data matrix and to exclude the top and bottom slices (which are sometimes affected by the registration procedures).

Once completed, the user has the option of saving the results to an R object or viewing the estimated components. The slices of each component map are plotted sequentially in a grid followed by the components associated time-course and that time-courses periodogram/power spectrum.

Value

User named R object (optional)

Once completed, the user has the option of saving the results to an R object named by the user.

Author(s)

J L Marchini <marchini@stats.ox.ac.uk> and C Heaton <chrisheaton99@yahoo.com>

See Also

[f.ica.fmri](#), [f.plot.ica.fmri](#)

<code>f.icast.fmri</code>	<i>Applies Spatial or Temporal ICA (Independent Component Analysis) to fMRI NIFTI datasets</i>
---------------------------	--

Description

Decomposes an fMRI dataset into a specified number of Spatially or Temporally Independent Components maps and associated time-courses using the FastICA algorithm

Usage

```
f.icast.fmri(foncfile,maskfile,is.spatial,n.comp.compute=TRUE,n.comp=0, hp.filter=TF
```

Arguments

<code>foncfile</code>	path and filename to fMRI dataset (NIFTI format .img or .nii file)
<code>maskfile</code>	path and filename to fMRI maskfile (0 and 1 values to determine if you are inside or outside the brain) dataset (NIFTI format .img or .nii file)
<code>is.spatial</code>	Logical. Should we perform a spatial or temporal ICA.
<code>n.comp.compute</code>	Logical. Should we estimate the number of components to extract. If FALSE, n.comp value (>0) should be provided
<code>n.comp</code>	number of components to extract
<code>hp.filter</code>	Logical. Should we perform high-pass filtering on the data

Details

TODO!!! The fMRI dataset is rearranged into a 2-dimensional data matrix X , where the column vectors are voxel time-series. A mask is used to specify which voxels are included. If this is not supplied by the user then a mask is constructed automatically using a 10% intensity threshold.

The data matrix is considered to be a linear combination of non-Gaussian (independent) components i.e. $X = AS$ where rows of S contain the independent components and A is a linear mixing matrix. In short ICA attempts to 'un-mix' the data by estimating an un-mixing matrix U where $UX = S$.

Under this generative model the measured 'signals' in X will tend to be 'more Gaussian' than the source components (in S) due to the Central Limit Theorem. Thus, in order to extract the independent components/sources we search for an un-mixing matrix U that maximizes the non-gaussianity of the sources.

In FastICA, non-gaussianity is measured using approximations to negentropy (J) which are more robust than kurtosis based measures and fast to compute.

The approximation takes the form

$$J(y) = [EG(y) - EG(v)]^2 \text{ where } v \text{ is a } N(0,1) \text{ r.v}$$

The following choices of G are included as options $G(u) = \frac{1}{\alpha} \log \cosh(\alpha u)$ and $G(u) = -\exp(\frac{-u^2}{2})$

The FastICA algorithm is used to 'un-mix' the data and recover estimates of the mixing matrix A and the source matrix S . Rows of the source matrix S represent spatially independent components of the dataset (these are arranged spatially in the output). Columns of A contain the associated time-courses of the independent components.

Pre-processing involves removing the mean of each row of the data matrix and (optionally) standardizing the columns of the data matrix to have zero mean and unit variance.

All computations are done using C code. This avoids reading the entire dataset into R and thus saves memory space.

Value

Nothing for the moment ... TODO!! The spatial and temporal components are written on disk

Author(s)

P Lafaye de Micheaux <plafaye@club.fr>

References

A. Hyvarinen and E. Oja (2000) Independent Component Analysis: Algorithms and Applications, Neural Networks, 13(4-5):411-430

Beckmann C. (2000) Independent Component Analysis for fMRI. First Year D.Phil Report, Dept. of Engineering Science, University of Oxford.

See Also

[f.icast.fmri.gui](#)

`f.icast.fmri.gui` *tcltk GUI to apply Spatial or Temporal ICA to fMRI NIFTI datasets*

Description

The GUI provides a quick and easy to use interface for applying spatial or temporal ICA to fMRI NIFTI datasets. Computations WILL BE (NOT YET IMPLEMENTED) done in C for speed and low memory usage.

Usage

```
f.icast.fmri.gui()
```

Details

The user is required to enter the location of the fMRI dataset (stored in the NIFTI format) and (optionally) a mask for the dataset. If no mask is supplied then an option to create mask is available. TODO!!

Once completed, the user has the option of saving the results to an R object or viewing the estimated components. The slices of each component map are plotted sequentially in a grid followed by the components associated time-course and that time-courses periodogram/power spectrum. TODO!!

Value

User named R object (optional)

Once completed, the user has the option of saving the results to an R object named by the user. TODO!!

Author(s)

P Lafaye de Micheaux <plafaye@club.fr>

See Also

[f.icast.fmri](#), [f.ica.fmri.gui](#)

`f.nifti.file.summary`

prints summary of .img file contents

Description

Prints a summary of the contents of a NIFTI .img file using the associated .hdr header file.

Usage

```
f.nifti.file.summary(file)
```

Arguments

file The location of .img file to be read

Value

A print out containing information about the .img file. This includes File name, Data Dimension, X dimension, Y dimension, Z dimension, Time dimension, Voxel dimensions, Data type

See Also

```
f.read.nifti.header, f.read.nifti.slice, f.read.nifti.slice.at.all.timepoints,  
f.read.nifti.ts, f.write.nifti, f.read.nifti.volume, f.spectral.summary.nifti,  
f.write.array.to.img.2bytes, f.write.array.to.img.float, f.write.list.to.hdr.nifti,  
f.basic.hdr.nifti.list.create
```

Examples

```
f.nifti.file.summary(system.file("example-nifti.img", package="AnalyzefMRI"))
```

f.plot.ica.fmri *Plots a specified component from the output of f.ica.fmri*

Description

Plots a specified component from the output of f.ica.fmri

Usage

```
f.plot.ica.fmri(obj.ica, comp, cols)
```

Arguments

obj.ica R object returned by the function f.ica.fmri
comp number of the component to plot
cols optional vector of colours to use for plotting

Details

The slices of the specified component map are plotted sequentially in a grid followed by the components associated time-course and that time-courses periodogram/power spectrum

Author(s)

J L Marchini <marchini@stats.ox.ac.uk> and C Heaton <chrisheaton99@yahoo.com>

See Also

[f.ica.fmri](#), [f.ica.fmri.gui](#)

```
f.plot.ica.fmri.jpg
```

Plot the components of the output of f.ica.fmri to a series of jpeg files

Description

This function allows the compact graphical storage of the output of a spatial ICA decomposition of an fMRI dataset. each component is plotted to a jpeg.

Usage

```
f.plot.ica.fmri.jpg(ica.obj, file="./ica", cols=heat.colors(100), width=700, height=700)
```

Arguments

ica.obj	Object that is the output of f.ica.fmri
file	The component i will be plotted in file file.comp.i.jpeg
cols	Optional colour vector for plotting the components
width	Width of jpeg images
height	Height of jpeg images

Author(s)

J L Marchini

See Also

[f.ica.fmri](#), [jpeg](#)

```
f.plot.volume.gui tcltk GUI to display FMRI or MRI images
```

Description

tcltk GUI to display FMRI or MRI images. This GUI is very usefull, for example, for investigating the results of an ICA performed with f.icast.fmri.gui(). But it can also be used to display an MRI or an FMRI image

Usage

```
f.plot.volume.gui()
```

Details

One has the possibility to enter either a filename (with its path) or directly an R object in the file field.

Value

Nothing

Author(s)

P Lafaye de Micheaux <plafaye@club.fr>

See Also

`f.icast.fmri.gui`

Examples

```
# TODO!!
```

```
f.read.analyze.header
      read Analyze header file
```

Description

Reads the ANALYZE image format .hdr header file into a list.

Usage

```
f.read.analyze.header(file)
```

Arguments

<code>file</code>	The .hdr file to be read
-------------------	--------------------------

Value

A list containing the information in the fields of the .hdr file.

<code>file.name</code>	path name of the .img file
<code>swap</code>	TRUE or FALSE variable indicating whether files are big or little endian
<code>sizeof.hdr</code>	Must indicate the byte size of the header file
<code>data.type</code>	character vector indicating data storage type for each voxel
<code>db.name</code>	
<code>extents</code>	Should be 16384, the image file is created as contiguous with a minimum extent size

```

session.error

regular      Must be 'r' to indicate that all images and volumes are the same size
hkey.un0
dim          vector of the image dimensions: dim[1] Number of dimensions in database, usu-
ally 4; dim[2] Image X dimension; number of pixels in an image row; dim[3]
Image Y dimension; number of pixel rows in slice; dim[4] Volume Z dimen-
sion, number of slices in a volume; dim[5] Time points, number of volumes in
database

vox.units    specifies the spatial units of measure for a voxel
cal.units    specifies the name of the calibration unit i.e. pixel,voxel
unused1
datatype    integer indicator of data storage type for this image
bitpix      number of bits per pixel: 1, 8, 16, 32, or 64
dim.un0     unused
pixdim      Parallel vector to dim, giving real world measurements in mm. and ms. pixdim[1]:
voxel width in mm. pixdim[2]: voxel height in mm. pixdim[3]: slice thickness
in mm.

vox.offset   byte offset in the .img file at which voxels start. This value can be negative to
specify that the absolute value is applied for every image in the file

scale       specify the range of calibration values. SPM extends the Analyze format by
using a scaling factor for the image from the header

funused2
funused3
cal.max     Max display intensity
cal.min     Min display intensity
compressed
verified
glmax       The maximum pixel values for the entire database
glmin      The minimum pixel values for the entire database
descrip     any text you like
aux.file    auxiliary filename
orient      slice orientation for this dataset: 0 transverse unflipped; 1 coronal unflipped; 2
sagittal unflipped; 3 transverse flipped; 4 coronal flipped; 5 sagittal flipped

originator  image central voxel coordinates. SPM uses this Analyze header field in an un-
orthodox way

generated
scannum
patient.id
exp.date

```

```
exp.time  
hist.un0  
views  
vols.added  
start.field  
field.skip  
omax  
omin  
smax  
smin
```

See Also

[f.analyze.file.summary](#)

Examples

```
f.read.analyze.header(system.file("example.hdr", package="AnalyzeFMRI"))
```

```
f.read.analyze.slice  
                  read one slice from a .img file
```

Description

Reads in a specific slice from an ANALYZE .img image format file into an array.

Usage

```
f.read.analyze.slice(file, slice, tpt)
```

Arguments

file	The .img file to be read from
slice	The number of the slice (assumed to be the 3rd dimension)
tpt	The number of the scan that the slice is to be taken from

Details

The entire dataset is assumed to be 4D and a slice is extracted that is referenced by specifying the last two dimensions of the dataset i.e.slice and tpt.

Value

An array containing the slice

See Also

[f.read.analyze.slice.at.all.timepoints](#), [f.read.analyze.ts](#), [f.read.analyze.volume](#)

Examples

```
a<-f.read.analyze.slice(system.file("example.img", package="AnalyzeFMRI"),10,1)
dim(a)
```

```
f.read.analyze.slice.at.all.timepoints
```

reads a slice at all time points from a .img file

Description

Reads in a slice of a .img file at all time points into an array

Usage

```
f.read.analyze.slice.at.all.timepoints(file, slice)
```

Arguments

<code>file</code>	<code>file</code> The location of the .img file
<code>slice</code>	<code>slice</code> The number of the slice to be read in

Value

An array containing the slice at all time points

See Also

[f.read.analyze.slice](#), [f.read.analyze.ts](#), [f.read.analyze.volume](#)

Examples

```
a<-f.read.analyze.slice.at.all.timepoints(system.file("example.img", package="AnalyzeFMRI"),
dim(a))
```

f.read.analyze.tpt *Read in a volume at one time point*

Description

Given a 4D ANALYZE .img/.hdr image pair this function can read in the 3D volume of measurements at a specific time point.

Usage

```
f.read.analyze.tpt(file, tpt)
```

Arguments

file	The .img file.
tpt	The time point to read in.

Details

Given a 4D ANALYZE .img/.hdr image pair this function can read in the 3D volume of measurements at a specific time point.

Value

A 3D array containing the volume.

See Also

[f.read.analyze.slice](#), [f.read.analyze.slice.at.all.timepoints](#), [f.write.analyze](#),

Examples

```
f.read.analyze.tpt(system.file("example.img", package="AnalyzeFMRI"), 1)
```

f.read.analyze.ts *read in one voxel time series*

Description

Given a 4D ANALYZE .img/.hdr image pair this function can read in the time series from a specified position in 3D into a vector.

Usage

```
f.read.analyze.ts(file, x, y, z)
```

Arguments

file	The .img file
x	The x-coordinate
y	The y-coordinate
z	The z-coordinate

Details

Given a 4D ANALYZE .img/.hdr image pair this function can read in the time series from a specified position in 3D into a vector.

Value

A vector containing the time series

See Also

[f.read.analyze.slice](#), [f.read.analyze.slice.at.all.timepoints](#), [f.write.analyze](#),

Examples

```
f.read.analyze.ts(system.file("example.img", package="AnalyzeFMRI"), 30, 30, 10)
```

```
f.read.analyze.volume  
    read whole .img file
```

Description

Reads the ANALYZE image format .img file into an array.

Usage

```
f.read.analyze.volume(file)
```

Arguments

file	The location of the .img file to be read
------	--

Value

An array with the appropriate dimensions containing the image volume. A print out of the file information is also given. The function assumes that the corresponding .hdr file is in the same directory as the .img file.

See Also

[f.read.analyze.slice](#), [f.read.analyze.slice.at.all.timepoints](#), [f.read.analyze.ts](#)

Examples

```
a<-f.read.analyze.volume(system.file("example.img", package="AnalyzeFMRI"))
dim(a)
```

f.read.header	<i>read ANALYZE or NIFTI header file</i>
---------------	--

Description

Reads the ANALYZE or NIFTI image format .hdr header file into a list. The format type is determined by first reading the magic field.

Usage

```
f.read.header(file)
```

Arguments

file The .hdr file to be read

Value

A list containing the information in the fields of the .hdr file. See [f.read.analyze.header](#) of [f.read.nifti.header](#) to have the list of values.

See Also

[f.read.analyze.header](#) [f.read.nifti.header](#)

Examples

```
f.read.header(system.file("example.hdr", package="AnalyzeFMRI"))
f.read.header(system.file("example-nifti.hdr", package="AnalyzeFMRI"))
```

```
f.read.nifti.header
      read Nifti header file
```

Description

Reads the NIFTI image format .hdr header file into a list.

Usage

```
f.read.nifti.header(file)
```

Arguments

file The .hdr file to be read

Value

A list containing the information in the fields of the .hdr file.

file.name	path name of the .img file
swap	1 or 0 variable indicating whether files are big (=native) or little (=swapped) endian
sizeof.hdr	MUST be 348
data.type	char[10]. UNUSED
db.name	char[18]. UNUSED
extents	UNUSED
session.error	UNUSED
regular	UNUSED, but filled with 'r' as SPM does
dim.info	MRI slice ordering: This field encode which spatial dimension (1=x, 2=y, or 3=z) corresponds to which acquisition dimension for MRI data. In fact, it contains three informations: freq.dim, phase.dim and slice.dim, all squished into the single byte field dim.info (2 bits each, since the values for each field are limited to the range 0..3). The R function diminfo2fps can be used to extract these values from the dim.info byte.
dim	vector (of length 8) of image dimensions. dim[1] specifies the number of dimensions. In NIFTI-1 files, dim[2], dim[3], dim[4] are for space, dim[5] is for time. The 5th dimension (dim[6]) of the dataset, if present (i.e., dim[1]=5 and dim[6] > 1), contains multiple values (for example a vector) to be stored at each spatiotemporal location. Uses of dim[7] and dim[8] are not specified in NIFTI-1 format.
intent.p1	1st intent parameter: first auxiliary parameter for a possible statistical distribution specified in intent.code

<code>intent.p2</code>	2nd intent parameter: second auxiliary parameter for a possible statistical distribution specified in <code>intent.code</code>
<code>intent.p3</code>	3rd intent parameter: third auxiliary parameter for a possible statistical distribution specified in <code>intent.code</code>
<code>intent.code</code>	NIFTI INTENT code: if 0, this is a raw dataset; if in range 2...24, this indicates that the numbers in the dataset should be interpreted as being drawn from a given distribution. Most such distributions have auxiliary parameters (given with <code>intent.p?</code>); if in range 1001...1011, this is an other meaning. See file <code>intent-code.txt</code> in the <code>niftidoc</code> directory of the source package. If the dataset DOES NOT have a 5th dimension (<code>dim[1]=4</code>), then the auxiliary parameters are the same for each voxel, and are given in header fields <code>intent.p1</code> , <code>intent.p2</code> , and <code>intent.p3</code> . If the dataset DOES have a 5th dimension (<code>dim[1]=5</code>), then the auxiliary parameters are different for each voxel.
<code>datatype</code>	integer indicator of data storage type for each voxel. This could be 2 (unsigned char), 4 (signed short), 8 (signed int), 16 (32 bit float), 32 (64 bit complex = two 32 bit floats), 64 (64 bit float = double), 128 (3 8 bit bytes), 256 (signed char), 512 (unsigned short), 768 (unsigned int), 1024 (signed long long), 1280 (unsigned long long), 1536 (128 bit float = long double), 1792 (128 bit complex = 2 64 bit floats), 2048 (256 bit complex = 2 128 bit floats).
<code>bitpix</code>	the number of bits per voxel. This field MUST correspond with the <code>datatype</code> field. The total number of bytes in the image data is $\text{dim}[2] * \dots * \text{dim}[\text{dim}[1]+1] * \text{bitpix} / 8$
<code>slice.start</code>	Indicates the start of the slice acquisition pattern, when <code>slice.code</code> is nonzero. These values are present to allow for the possible addition of "padded" slices at either end of the volume, which don't fit into the slice timing pattern. If there are no padding slices, then <code>slice.start=0</code> and <code>slice.end=dim[slice.dim+1]-1</code> are the correct values. For these values to be meaningful, <code>slice.start</code> must be non-negative and <code>slice.end</code> must be greater than <code>slice.start</code> .
<code>pixdim</code>	vector (of length 8). Grid spacings. When reading a NIFTI-1 header, <code>pixdim[1]</code> stores <code>qfac</code> (which is either -1 or 1). If <code>pixdim[1]=0</code> (which should not occur), we take <code>qfac=1</code> . <code>pixdim[2]</code> , <code>pixdim[3]</code> and <code>pixdim[4]</code> give the voxel width along dimension x, y and z respectively. <code>pixdim[5]</code> gives the time step (=Time Repetition=TR). The units of <code>pixdim</code> can be specified with the <code>xyzt.units</code> field.
<code>vox.offset</code>	Offset into <code>.nii</code> file. Should be 352 for a <code>.nii</code> file, 0 for a <code>nifti .hdr/.img</code> pair.
<code>scl.slope</code>	Data scaling: If the <code>scl.slope</code> field is nonzero, then each voxel value in the dataset should be scaled as $y = \text{scl.slope} * x + \text{scl.inter}$, where x = voxel value stored and y = "true" voxel value
<code>scl.inter</code>	Data scaling: offset. Idem above.
<code>slice.end</code>	Indicates the end of the slice acquisition pattern, when <code>slice.code</code> is nonzero. These values are present to allow for the possible addition of "padded" slices at either end of the volume, which don't fit into the slice timing pattern. If there are no padding slices, then <code>slice.start=0</code> and <code>slice.end=dim[slice.dim+1]-1</code> are the correct values. For these values to be meaningful, <code>slice.start</code> must be non-negative and <code>slice.end</code> must be greater than <code>slice.start</code> .
<code>slice.code</code>	Slice timing order. If this is nonzero, AND if <code>slice.dim</code> is nonzero, AND if <code>slice.duration</code> is positive, indicates the timing pattern of the slice acquisition.

The following codes are defined: 0 (NIFTI SLICE UNKNOWN), 1 (NIFTI SLICE SEQ INC), 2 (NIFTI SLICE SEQ DEC), 3 (NIFTI SLICE ALT INC), 4 (NIFTI SLICE ALT DEC)

<code>xyzt.units</code>	Units of <code>pixdim[2:5]</code> . Bits 1..3 of <code>xyzt.units</code> specify the (same) space unit of <code>pixdim[2:4]</code> . Bits 4..6 of <code>xyzt.units</code> specify the time unit of <code>pixdim[5]</code> . See <code>xyzt-units.txt</code> in the <code>niftidoc</code> directory of the source package. The R function <code>xyzt2st</code> can be used to extract these values from the <code>xyzt.units</code> byte.
<code>cal.max</code>	Maximum display intensity (white) corresponds to dataset value <code>cal.max</code> . Dataset values above <code>cal.max</code> should display as white. <code>cal.min</code> and <code>cal.max</code> only make sense when applied to scalar-valued datasets (i.e., <code>dim[1] < 5</code> or <code>dim[6] = 1</code>).
<code>cal.min</code>	Minimum display intensity (black) corresponds to dataset value <code>cal.min</code> . Dataset values below <code>cal.min</code> should display as black.
<code>slice.duration</code>	Time for 1 slice. If this is positive, AND if <code>slice.dim</code> is nonzero, indicates the amount of time used to acquire 1 slice.
<code>toffset</code>	Time axis shift: The <code>toffset</code> field can be used to indicate a nonzero start point for the time axis. That is, time point <code>m</code> is at <code>t=toffset+m*pixdim[5]</code> for <code>m=1, ..., dim[5]-1</code> .
<code>glmax</code>	UNUSED
<code>glmin</code>	UNUSED
<code>descrip</code>	<code>char[80]</code> . This field may contain any text you like
<code>aux.file</code>	<code>char[24]</code> . This field is used to store an auxiliary filename.
<code>qform.code</code>	NIFTI code (in 0, ... ,4). 0: Arbitrary coordinates; 1: Scanner-based anatomical coordinates; 2: Coordinates aligned to another file's, or to anatomical "truth" (coregistration); 3: Coordinates aligned to Talairach-Tournoux Atlas; 4: MNI 152 normalized coordinates
<code>sform.code</code>	NIFTI code (in 0, ... ,4) with the same meaning as <code>qform</code> codes. The basic idea behind having two coordinate systems is to allow the image to store information about (1) the scanner coordinate system used in the acquisition of the volume (in the <code>qform</code>) and (2) the relationship to a standard coordinate system - e.g. MNI coordinates (in the <code>sform</code>). The <code>qform</code> allows orientation information to be kept for alignment purposes without losing volumetric information, since the <code>qform</code> only stores a rigid-body transformation (rotation and translation) which preserves volume. On the other hand, the <code>sform</code> stores a general affine transformation (shear, scale, rotation and translation) which can map the image coordinates into a standard coordinate system, like Talairach or MNI, without the need to resample the image. By having both coordinate systems, it is possible to keep the original data (without resampling), along with information on how it was acquired (<code>qform</code>) and how it relates to other images via a standard space (<code>sform</code>). This ability is advantageous for many analysis pipelines, and has previously required storing additional files along with the image files. By using NIfTI-1 this extra information can be kept in the image files themselves. Note: the <code>qform</code> and <code>sform</code> also store information on whether the coordinate system is left-handed or right-handed and so when both are set they must be consistent, otherwise the handedness of the coordinate system (often used to distinguish

	left-right order) is unknown and the results of applying operations to such an image are unspecified.
quatern.b	Quaternion b param. These b,c,d quaternion parameters encode a rotation matrix used when qform.code > 0 to obtain a rigid transformation that maps voxel indices (i,j,k) to spatial coordinates (x,y,z), typically anatomical coordinates assigned by the scanner. This transformation ("Method 2" in the nifti1.h documentation) is generated using also the voxel dimensions (pixdim[1:4]) and a 3D shift, i.e. a translation, (qoffset.*)
quatern.c	Quaternion c param
quatern.d	Quaternion d param
qoffset.x	Quaternion x shift. If the (0020,0032) DICOM attribute is extracted into (px,py,pz), then qoffset.x = -px qoffset.y = -py qoffset.z = pz is a reasonable setting when qform.code=NIFTI XFORM SCANNER ANAT.
qoffset.y	Quaternion y shift
qoffset.z	Quaternion z shift
srow.x	vector of length 4. 1st row affine transform. These srow.* parameters contain an affine (non-rigid) transformation ("Method 3" in the nifti1.h documentation) that maps voxel indices (i,j,k) to spatial coordinates (x,y,z).
srow.y	vector of length 4. 2nd row affine transform
srow.z	vector of length 4. 3rd row affine transform
intent.name	char[16]. 'name' or meaning of data. If no data name is implied or needed, intent.name[1] should be set to 0.
magic	MUST be "ni1" or "n+1"

Examples

```
f.read.nifti.header(system.file("example-nifti.hdr", package="AnalyzeFMRI"))
```

```
f.read.nifti.slice read one slice from a .img file in NIFTI format
```

Description

Reads in a specific slice from a NIFTI .img image format file into an array.

Usage

```
f.read.nifti.slice(file, slice, tpt)
```

Arguments

file	The .img file to be read from
slice	The number of the slice (assumed to be the 3rd dimension)
tpt	The number of the scan that the slice is to be taken from

Details

The entire dataset is assumed to be 4D and a slice is extracted that is referenced by specifying the last two dimensions of the dataset i.e.slice and tpt.

Value

An array containing the slice

See Also

[f.read.nifti.slice.at.all.timepoints](#), [f.read.nifti.ts](#), [f.read.nifti.volume](#)

Examples

```
a<-f.read.nifti.slice(system.file("example-nifti.img", package="AnalyzeFMRI"),10,1)
dim(a)
```

```
f.read.nifti.slice.at.all.timepoints
```

reads a slice at all time points from a NIFTI .img file

Description

Reads in a slice of a .img file at all time points into an array

Usage

```
f.read.nifti.slice.at.all.timepoints(file, slice)
```

Arguments

<code>file</code>	<code>file</code> The location of the .img file
<code>slice</code>	<code>slice</code> The number of the slice to be read in

Value

An array containing the slice at all time points

See Also

[f.read.nifti.slice](#), [f.read.nifti.ts](#), [f.read.nifti.volume](#)

Examples

```
a<-f.read.nifti.slice.at.all.timepoints(system.file("example-nifti.img", package="AnalyzeFMRI"),10,1)
dim(a)
```

f.read.nifti.tpt *Read in a volume at one time point*

Description

Given a 4D NIFTI .img/.hdr image pair this function can read in the 3D volume of measurements at a specific time point.

Usage

```
f.read.nifti.tpt(file, tpt)
```

Arguments

file	The .img file.
tpt	The time point to read in.

Details

Given a 4D NIFTI .img/.hdr image pair this function can read in the 3D volume of measurements at a specific time point.

Value

A 3D array containing the volume.

See Also

[f.read.nifti.slice](#), [f.read.nifti.slice.at.all.timepoints](#), [f.write.nifti](#),

Examples

```
f.read.nifti.tpt(system.file("example-nifti.img", package="AnalyzeFMRI"), 1)
```

f.read.nifti.ts *read in one voxel time series*

Description

Given a 4D NIFTI .img/.hdr image pair this function can read in the time series from a specified position in 3D into a vector.

Usage

```
f.read.nifti.ts(file, x, y, z)
```

Arguments

<code>file</code>	The .img file
<code>x</code>	The x-coordinate
<code>y</code>	The y-coordinate
<code>z</code>	The z-coordinate

Details

Given a 4D NIFTI .img/.hdr image pair this function can read in the time series from a specified position in 3D into a vector.

Value

A vector containing the time series

See Also

`f.read.nifti.slice`, `f.read.nifti.slice.at.all.timepoints`, `f.write.nifti`,

Examples

```
f.read.nifti.ts(system.file("example-nifti.img", package="AnalyzeFMRI"), 30, 30, 10)
```

```
f.read.nifti.volume  
    read whole image file
```

Description

Reads the NIFTI image file into an array.

Usage

```
f.read.nifti.volume(file)
```

Arguments

<code>file</code>	The location of the image file to be read
-------------------	---

Value

An array with the appropriate dimensions containing the image volume. A print out of the file information is also given. The function assumes that the corresponding .hdr file is in the same directory as the .img file (but if a .nii file is provided).

See Also

[f.read.nifti.slice](#), [f.read.nifti.slice.at.all.timepoints](#), [f.read.nifti.ts](#)

Examples

```
a<-f.read.nifti.volume(system.file("example-nifti.img", package="AnalyzeFMRI"))
dim(a)
```

<code>f.read.volume</code>	<i>read whole image file</i>
----------------------------	------------------------------

Description

Reads the ANALYZE or NIFTI image format image file into an array. Autodetects format type.

Usage

```
f.read.volume(file)
```

Arguments

`file` The location of the image file to be read

Value

An array with the appropriate dimensions containing the image volume. A print out of the file information is also given. The function assumes that the corresponding .hdr file is in the same directory as the .img file. (but if it is a .nii file)

See Also

[f.read.nifti.slice](#), [f.read.nifti.slice.at.all.timepoints](#), [f.read.nifti.ts](#)

Examples

```
a<-f.read.volume(system.file("example-nifti.img", package="AnalyzeFMRI"))
dim(a)
```

`f.spectral.summary` *plots graphical summary of spectral properties of an fMRI dataset*

Description

For an analyze .img file the periodogram of the time series are divided by a flat spectral estimate using the median periodogram ordinate. The resulting values are then combined within each Fourier frequency and quantiles are plotted against frequency. This provides a fast look at a fMRI dataset to identify any artifacts that reside at single frequencies.

Usage

```
f.spectral.summary(file, mask.file, ret.flag=FALSE)
```

Arguments

<code>file</code>	<code>file</code> The location of .img file
<code>mask.file</code>	<code>mask.file</code> Optional location of a .img file containing a mask. If not given then one is created.
<code>ret.flag</code>	<code>ret.flag</code> flag specifying whether to return the array of quantiles at each frequency

Value

If `ret.flag = TRUE` the an array of quantiles at each frequency is returned

See Also

[f.analyze.file.summary](#)

`f.spectral.summary.nifti`
plots graphical summary of spectral properties of an fMRI dataset

Description

For a NIFTI .img file the periodogram of the time series are divided by a flat spectral estimate using the median periodogram ordinate. The resulting values are then combined within each Fourier frequency and quantiles are plotted against frequency. This provides a fast look at a fMRI dataset to identify any artifacts that reside at single frequencies.

Usage

```
f.spectral.summary.nifti(file, mask.file, ret.flag=FALSE)
```

Arguments

file	file	The location of .img file
mask.file	mask.file	Optional location of a .img file containing a mask. If not given then one is created.
ret.flag	ret.flag	flag specifying whether to return the array of quantiles at each frequency

Value

If `ret.flag = TRUE` the an array of quantiles at each frequency is returned

See Also

[f.nifti.file.summary](#)

`f.write.analyze` *writes an array to a .img/.hdr pair in ANALYZE format*

Description

Creates a .img and .hdr pair of files from a given array

Usage

```
f.write.analyze(mat, file, size, pixdim, vox.units, cal.units, originator)
```

Arguments

mat	An array
file	The name of the file to be written, without .img or .hdr suffix
size	Specify the format of the .img file. Either "float" (for 4 byte floats) or "int" (2 byte integers) or "char" (1 byte integers).
pixdim	A vector of length 3 specifying the voxel dimensions in mm
vox.units	String specifying the spatial units of measure for a voxel
cal.units	String specifying the name of calibration unit
originator	vector of length 5, only the three first values are used. Put the last two equal to zero

Value

Nothing is returned

See Also

[f.write.array.to.img.8bit](#), [f.write.array.to.img.2bytes](#), [f.write.array.to.img.float](#)

Examples

```
a<-array(rnorm(20*30*40*3),dim=c(20,30,40,3))
file<-"temp"
f.write.analyze(a,file,size="float")
f.analyze.file.summary("temp.img")
```

```
f.write.array.to.img.2bytes
      write array of 2 byte integers
```

Description

Writes an array to a .img file of 2 byte integers

Usage

```
f.write.array.to.img.2bytes(mat,file)
```

Arguments

mat	An array
file	The name of the file to be written, preferably with .img suffix

Value

Nothing is returned

See Also

[f.write.analyze](#) [f.write.array.to.img.float](#)

```
f.write.array.to.img.8bit
      write array of 1 byte integers
```

Description

Writes an array to a .img file of 1 byte integers

Usage

```
f.write.array.to.img.8bit(mat,file)
```

Arguments

<code>mat</code>	An array
<code>file</code>	The name of the file to be written, preferably with <code>.img</code> suffix

Value

Nothing is returned

See Also

[f.write.analyze](#), [f.write.array.to.img.float](#), [f.write.array.to.img.2bytes](#)

`f.write.array.to.img.float`
write array of 4 byte floats

Description

Writes an array to a `.img` file of 4 byte floats

Usage

`f.write.array.to.img.float(mat, file)`

Arguments

<code>mat</code>	An array
<code>file</code>	The name of the file to be written, preferably with <code>.img</code> suffix

Value

Nothing is returned

See Also

[f.write.analyze](#), [f.write.array.to.img.2bytes](#), [f.write.array.to.img.8bit](#)

```
f.write.list.to.hdr
```

writes a .hdr file in ANALYZE format

Description

Writes a list of attributes to a .hdr file

Usage

```
f.write.list.to.hdr(L, file)
```

Arguments

L	A list of all the fields included in a .hdr file
file	The name of the file to write, preferably with .hdr suffix

Value

Nothing is returned

See Also

[f.basic.hdr.list.create](#)

Examples

```
a<-array(rnorm(20*30*40*3), dim=c(20, 30, 40, 3))
file<-"temp.hdr"
b<-f.basic.hdr.list.create(a, file)
f.write.list.to.hdr(b, file)
```

```
f.write.list.to.hdr.nifti
```

writes a .hdr file in NIFTI format

Description

Writes a list of attributes to a .hdr file

Usage

```
f.write.list.to.hdr.nifti(L, file)
```

Arguments

L	A list of the all the fields included in a .hdr file
file	The name of the file to write, preferably with .hdr suffix

Value

Nothing is returned

See Also

[f.basic.hdr.nifti.list.create](#)

Examples

```
a<-array(rnorm(20*30*40*3),dim=c(20,30,40,3))
file<-"temp.hdr"
b<-f.basic.hdr.nifti.list.create(dim(a), file)
f.write.list.to.hdr.nifti(b, file)
```

f.write.nifti	<i>writes an array to a .img/.hdr pair in NIFTI format or to a .nii file</i>
---------------	--

Description

Creates a .img/.hdr pair of files or a .nii file from a given array

Usage

```
f.write.nifti(mat, file, size, L, nii)
```

Arguments

mat	An array
file	The name of the file to be written, without .img or .hdr suffix
size	Specify the format of the .img file. Either "float" (for 4 byte floats) or "int" (2 byte integers) or "char" (1 byte integers).
L	if NULL, the list is created by the function, else it should be provided. This list contains the header part of a NIFTI image.
nii	should we write only one .nii file or a .hdr/.img pair of files

Value

Nothing is returned

See Also

```
f.write.array.to.img.8bit, f.write.array.to.img.2bytes, f.write.array.to.img.float  
f.write.nii.array.to.img.8bit, f.write.nii.array.to.img.2bytes, f.write.nii.array.to.
```

Examples

```
a<-array(rnorm(20*30*40*3), dim=c(20, 30, 40, 3))  
file<-"temp"  
f.write.nifti(a, file, size="float", nii=TRUE)
```

```
f.write.nii.array.to.img.2bytes
```

write array of 2 byte integers and add at the beginning of the file the NIFTI header part

Description

Writes an array to a .img file of 2 byte integers and add at the beginning of the file the NIFTI header part

Usage

```
f.write.nii.array.to.img.2bytes(mat, L, file)
```

Arguments

mat	An array
L	A list containing the header information
file	The name of the file to be written, preferably with .img suffix

Value

Nothing is returned

See Also

```
f.write.nifti f.write.nii.array.to.img.float
```

```
f.write.nii.array.to.img.8bit
```

write array of 1 byte integers and add at the beginning of the file the NIFTI header part

Description

Writes an array to a .img file of 1 byte integers and add at the beginning of the file the NIFTI header part

Usage

```
f.write.nii.array.to.img.8bit(mat, L, file)
```

Arguments

<code>mat</code>	An array
<code>L</code>	A list containing the header information
<code>file</code>	The name of the file to be written, preferably with .img suffix

Value

Nothing is returned

See Also

[f.write.nifti](#), [f.write.nii.array.to.img.float](#), [f.write.nii.array.to.img.2bytes](#)

```
f.write.nii.array.to.img.float
```

write array of 4 byte floats and add at the beginning of the file the NIFTI header part

Description

Writes an array to a .img file of 4 byte floats and add at the beginning of the file the NIFTI header part

Usage

```
f.write.nii.array.to.img.float(mat, L, file)
```

Arguments

<code>mat</code>	An array
<code>L</code>	A list containing the header information
<code>file</code>	The name of the file to be written, preferably with <code>.img</code> suffix

Value

Nothing is returned

See Also

[f.write.nifti](#), [f.write.nii.array.to.img.2bytes](#), [f.write.nii.array.to.img.8bit](#)

fourDto2D

fourDto2D

Description

This function transform a 4D image in a 2D image matrix.

Usage

```
fourDto2D(volume.4d, tm)
```

Arguments

<code>volume.4d</code>	a 4D array to be transformed
<code>tm</code>	number of time dimensions

Value

`x.2d` matrix of size `tm x vm` which contains the `tm` images

See Also

[threeDto4D](#) [twoDto4D](#)

fps2diminfo	<i>fps2diminfo</i>
-------------	--------------------

Description

Encode freq.dim, phase.dim and slice.dim fields into the one byte dim.info field of a NIFTI header file.

Usage

```
fps2diminfo(freq.dim, phase.dim, slice.dim)
```

Arguments

freq.dim	freq.dim field of a NIFTI file
phase.dim	phase.dim field of a NIFTI file
slice.dim	slice.dim field of a NIFTI file

Value

A list containing dim.info field.

See Also

[diminfo2fps](#)

Examples

```
dim.info <- f.read.header(system.file("example-nifti.hdr", package="AnalyzeFMRI"))$dim.info
mylist <- diminfo2fps(dim.info)
fps2diminfo(mylist$freq.dim, mylist$phase.dim, mylist$slice.dim)
```

GaussSmoothArray	<i>Spatially smooth an array with Gaussian kernel.</i>
------------------	--

Description

Applies a stationary Gaussian spatial smoothing kernel to a 3D or 4D array.

Usage

```
GaussSmoothArray(x, voxdim=c(1, 1, 1), ksize=5, sigma=diag(3, 3), mask=NULL, var.no
```

Arguments

<code>x</code>	The array to be smoothed.
<code>voxdim</code>	The dimensions of the <i>volume elements</i> (voxel) that make up the array.
<code>ksize</code>	The dimensions (in number of voxels) of the 3D discrete smoothing kernel used to smooth the array.
<code>sigma</code>	The covariance matrix of the 3D Gaussian smoothing kernel. This matrix doesn't have to be non-singular; zero on the diagonal of <code>sigma</code> indicate no smoothing in that direction.
<code>mask</code>	A 3D 0-1 mask that delimits where the smoothing occurs.
<code>var.norm</code>	Logical flag indicating whether to normalize the variance of the smoothed array.

Value

The smoothed array is returned.

Author(s)

J. L. Msrchini

See Also

[GaussSmoothKernel](#)

Examples

```
d <- c(10, 10, 10, 20)
mat <- array(rnorm(cumprod(d)[length(d)]), dim = d)
mat[, , 6:10, ] <- mat[, , 6:10, ] + 3
mask <- array(0, dim = d[1:3])
mask[3:8, 3:8, 3:8] <- 1
b <- GaussSmoothArray(mat, mask = mask, voxdim = c(1, 1, 1), ksize = 5, sigma = diag(1, 3))
```

`GaussSmoothKernel` *Calculates a discrete Gaussian smoothing kernel.*

Description

Calculates a simple, discrete Gaussian smoothing kernel of a specific size given the covariance matrix of the Gaussian.

Usage

```
GaussSmoothKernel(voxdim=c(1, 1, 1), ksize=5, sigma=diag(3, 3))
```

Arguments

<code>voxdim</code>	Dimensions of each voxel.
<code>ksize</code>	Dimensions of the discrete kernel size.
<code>sigma</code>	The covariance matrix of the Gaussian kernel.

Value

An array of dimension (ksize,ksize,ksize) containing the smoothing kernel.

Author(s)

J. L. Marchini

Examples

```
a <- GaussSmoothKernel(voxdim=c(1,1,1), ksize=5, sigma=diag(1,3))
```

ICAspat

ICAspat

Description

This function performs a spatial ICA

Usage

```
ICAspat(X, n.comp, alg.typ="parallel", centering=TRUE, hp.filter=TRUE)
```

Arguments

<code>X</code>	a matrix of size $t_m \times v_m$ which contains the functional images
<code>n.comp</code>	number of maximally independent components to extract
<code>alg.typ</code>	if <code>'alg.typ == "parallel"</code> the components are extracted simultaneously (the default). if <code>'alg.typ == "deflation"</code> the components are extracted one at a time.
<code>centering</code>	Logical. Should we center the data first. Centering will be performed by firstly removing the column mean.
<code>hp.filter</code>	Logical. Should we perform high-pass filtering on the data

Value

A list containing

<code>time.series</code>	estimated mixing matrix of size $t_m \times n.comp$
<code>spatial.components</code>	estimated source matrix of size $n.comp \times v_m$

See Also[ICAtemp](#)**Examples**

```
# TODO!!
```

`ICAtemp`

ICAtemp

Description

This function performs a temporal ICA

Usage

```
ICAtemp(X, n.comp, alg.typ="parallel", centering=TRUE, hp.filter=TRUE)
```

Arguments

<code>X</code>	a matrix of size $v_m \times t_m$ which contains the functional images
<code>n.comp</code>	number of maximally independent components to extract
<code>alg.typ</code>	if <code>'alg.typ == "parallel"</code> the components are extracted simultaneously (the default). if <code>'alg.typ == "deflation"</code> the components are extracted one at a time.
<code>centering</code>	Logical. Should we center the data first. Centering will be performed by firstly removing the column mean.
<code>hp.filter</code>	Logical. Should we perform high-pass filtering on the data

Value

A list containing

<code>time.series</code>	estimated source matrix of size $n.comp \times t_m$
<code>spatial.components</code>	estimated mixing matrix of size $v_m \times n.comp$

See Also[ICAspat](#)**Examples**

```
# TODO!!
```

ijk2xyz

ijk2xyz

Description

This function maps from data coordinates (e.g. column *i*, row *j*, slice *k*), into some real world (*x,y,z*) positions in space. These positions could relate to Talairach-Tournoux (T&T) space, MNI space, or patient-based scanner coordinates.

Usage

```
ijk2xyz(ijk=c(1,1,1),method=2,L)
```

Arguments

<i>ijk</i>	matrix. Each column of <i>ijk</i> should contain a voxel index coordinates (<i>i,j,k</i>) to be mapped to its (<i>x,y,z</i>) real coordinates in some other space
<i>method</i>	1 (qform.code=sform.code=0), 2 (qform.code>0, rigid transformation) or 3 (sform.code>0, affine transformation).
<i>L</i>	header list of a NIFTI file

Details

The NIFTI format allows storage on disk to be in either a left- or right-handed coordinate system. However, the format includes an implicit spatial transformation into a RIGHT-HANDED coordinate system. This transform maps from data coordinates (e.g. column *i*, row *j*, slice *k*), into some real world (*x,y,z*) positions in space. These positions could relate to Talairach-Tournoux (T&T) space, MNI space, or patient-based scanner coordinates. For T&T, and MNI coordinates, *x* increases from left to right, *y* increases from posterior to anterior, and *z* increases in the inferior to superior direction. Directions in the scanner coordinate system are similar. MRI data is usually exported as DICOM format, which encodes the positions and orientations of the slices. When data are converted from DICOM to NIFTI-1 format, the relevant information can be determined from the Pixel Spacing, Image Orientation (Patient) and Image Position (Patient) fields of the DICOM files. NIFTI-1 also allows the space of one image to be mapped to that of another (via a rigid or affine transform). This is to enable on-the-fly resampling of registered images. This would allow intra-subject images, collected with lots of different orientations or resolutions, to be treated as if they are all in register.

Neurological and radiological conventions only relate to visualization of axial images. They are unrelated to how the data are stored on disk, or even how the real-world coordinates are represented. It is more appropriate to consider whether the real-world coordinate system is left- or right-handed (see below). Talairach and Tournoux use a right-handed system, whereas the storage convention of ANALYZE files is usually considered as left-handed. These coordinate systems are mirror images of each other (if you are a psychologist, try explaining why mirror images appear to be left-right flipped, rather than flipped up-down, or back-front). Transforming between left- and right-handed coordinate systems involves flipping, and can not be done by rotations alone.

x=pouce, *y*=index, *z*=majeur de la main gauche (resp. droite) pour les droitiers (resp. gauchers)

Volume orientation is given by a transformation that maps voxel indices (i,j,k) to spatial coordinates (x,y,z), typically anatomical coordinates assigned by the scanner. This transformation ("Method 2" in the nifti1.h documentation) is generated using the voxel dimensions, a quaternion encoding a rotation matrix, and a 3D shift, all stored in the NIFTI-1 header; details can be found in the nifti1.h comments. The NIFTI-1 header also provides for a general affine transformation, separate from that described by Method 2. This transformation ("Method 3") also maps voxel indices (i,j,k) to (x,y,z), which in this case are typically coordinates in a standard space such as the Talairach space. The elements of this transformation matrix are stored in the NIFTI-1 header. For example, the Method 2 transformation can be constructed from the attributes from a set of DICOM files; the Method 3 transform can be computed offline and inserted into the header later. The exact "meaning" of the coordinates given by the Method 2 and Method 3 transformations is recorded in header fields qform.code and sform.code, respectively. Code values can indicate if the (x,y,z) axes are Anatomical coordinates from the scanner (e.g., the DICOM header) Aligned to some anatomical "truth" or standard Aligned and warped to Talairach-Tournoux coordinates Aligned and warped to MNI-152 coordinates

It is possible that neither transformation is specified (i.e., qform.code=sform.code=0), in which case we are left with the voxel size in pixdim[], and no orientation is given or assumed. This use ("Method 1") is discouraged.

The basic idea behind having two coordinate systems is to allow the image to store information about (1) the scanner coordinate system used in the acquisition of the volume (in the qform) and (2) the relationship to a standard coordinate system - e.g. MNI coordinates (in the sform). The qform allows orientation information to be kept for alignment purposes without losing volumetric information, since the qform only stores a rigid-body transformation which preserves volume. On the other hand, the sform stores a general affine transformation which can map the image coordinates into a standard coordinate system, like Talairach or MNI, without the need to resample the image. By having both coordinate systems, it is possible to keep the original data (without resampling), along with information on how it was acquired (qform) and how it relates to other images via a standard space (sform). This ability is advantageous for many analysis pipelines, and has previously required storing additional files along with the image files. By using NIFTI-1 this extra information can be kept in the image files themselves. Note: the qform and sform also store information on whether the coordinate system is left-handed or right-handed (see Q15) and so when both are set they must be consistent, otherwise the handedness of the coordinate system (often used to distinguish left-right order) is unknown and the results of applying operations to such an image are unspecified.

There are 3 different methods by which continuous coordinates can be attached to voxels. The discussion below emphasizes 3D volumes, and the continuous coordinates are referred to as (x,y,z). The voxel index coordinates (i.e., the array indexes) are referred to as (i,j,k), with valid ranges: $i = 0 \dots \text{dim}[1]-1$ $j = 0 \dots \text{dim}[2]-1$ (if $\text{dim}[0] \geq 2$) $k = 0 \dots \text{dim}[3]-1$ (if $\text{dim}[0] \geq 3$) The (x,y,z) coordinates refer to the CENTER of a voxel. In methods 2 and 3, the (x,y,z) axes refer to a subject-based coordinate system, with +x = Right +y = Anterior +z = Superior. This is a right-handed coordinate system. However, the exact direction these axes point with respect to the subject depends on qform.code (Method 2) and sform.code (Method 3).

N.B.: The i index varies most rapidly, j index next, k index slowest. Thus, voxel (i,j,k) is stored starting at location $(i + j*\text{dim}[1] + k*\text{dim}[1]*\text{dim}[2]) * (\text{bitpix}/8)$ into the dataset array.

N.B.: The ANALYZE 7.5 coordinate system is +x = Left +y = Anterior +z = Superior which is a left-handed coordinate system. This backwardness is too difficult to tolerate, so this NIFTI-1 standard specifies the coordinate order which is most common in functional neuroimaging.

N.B.: The 3 methods below all give the locations of the voxel centers in the (x,y,z) coordinate

system. In many cases, programs will wish to display image data on some other grid. In such a case, the program will need to convert its desired (x,y,z) values into (i,j,k) values in order to extract (or interpolate) the image data. This operation would be done with the inverse transformation to those described below.

N.B.: Method 2 uses a factor 'qfac' which is either -1 or 1; qfac is stored in the otherwise unused pixdim[0]. If pixdim[0]=0.0 (which should not occur), we take qfac=1. Of course, pixdim[0] is only used when reading a NIFTI-1 header, not when reading an ANALYZE 7.5 header.

N.B.: The units of (x,y,z) can be specified using the xyzt.units field.

METHOD 1 (the "old" way, used only when qform.code = 0): _____
 _____ The coordinate mapping from (i,j,k) to (x,y,z) is the ANALYZE 7.5 way. This is a simple scaling relationship:

$$x = \text{pixdim}[1] * i \quad y = \text{pixdim}[2] * j \quad z = \text{pixdim}[3] * k$$

No particular spatial orientation is attached to these (x,y,z) coordinates. (NIFTI-1 does not have the ANALYZE 7.5 orient field, which is not general and is often not set properly.) This method is not recommended, and is present mainly for compatibility with ANALYZE 7.5 files.

METHOD 2 (used when qform.code > 0, which should be the "normal" case): _____
 _____ The (x,y,z) coordinates are given by the pixdim[] scales, a rotation matrix, and a shift. This method is intended to represent "scanner-anatomical" coordinates, which are often embedded in the image header (e.g., DICOM fields (0020,0032), (0020,0037), (0028,0030), and (0018,0050)), and represent the nominal orientation and location of the data. This method can also be used to represent "aligned" coordinates, which would typically result from some post-acquisition alignment of the volume to a standard orientation (e.g., the same subject on another day, or a rigid rotation to true anatomical orientation from the tilted position of the subject in the scanner). The formula for (x,y,z) in terms of header parameters and (i,j,k) is:

$$\begin{bmatrix} x \\ y \\ z \end{bmatrix} = \begin{bmatrix} R11 & R12 & R13 \\ R21 & R22 & R23 \\ R31 & R32 & R33 \end{bmatrix} \begin{bmatrix} \text{pixdim}[1] * i \\ \text{pixdim}[2] * j \\ \text{qfac} * \text{pixdim}[3] * k \end{bmatrix} + \begin{bmatrix} \text{qoffset.x} \\ \text{qoffset.y} \\ \text{qoffset.z} \end{bmatrix}$$

The qoffset.* shifts are in the NIFTI-1 header. Note that the center of the (i,j,k)=(0,0,0) voxel (first value in the dataset array) is just (x,y,z)=(qoffset.x,qoffset.y,qoffset.z).

The rotation matrix R is calculated from the quatern.* parameters. This calculation is described below.

The scaling factor qfac is either 1 or -1. The rotation matrix R defined by the quaternion parameters is "proper" (has determinant 1). This may not fit the needs of the data; for example, if the image grid is i increases from Left-to-Right j increases from Anterior-to-Posterior k increases from Inferior-to-Superior Then (i,j,k) is a left-handed triple. In this example, if qfac=1, the R matrix would have to be

$$\begin{bmatrix} 1 & 0 & 0 \\ 0 & -1 & 0 \\ 0 & 0 & 1 \end{bmatrix} \text{ which is "improper" (determinant} = -1). \begin{bmatrix} 0 & 0 & 1 \\ 0 & -1 & 0 \\ 1 & 0 & 0 \end{bmatrix}$$

If we set qfac=-1, then the R matrix would be

$$\begin{bmatrix} 1 & 0 & 0 \\ 0 & -1 & 0 \\ 0 & 0 & -1 \end{bmatrix} \text{ which is proper. } \begin{bmatrix} 0 & 0 & -1 \\ 0 & -1 & 0 \\ 1 & 0 & 0 \end{bmatrix}$$

This R matrix is represented by quaternion [a,b,c,d] = [0,1,0,0] (which encodes a 180 degree rotation about the x-axis).

METHOD 3 (used when sform.code > 0): _____ The (x,y,z) coordinates are given by a general affine transformation of the (i,j,k) indexes:

$$\begin{aligned} x &= \text{srow.x}[0] * i + \text{srow.x}[1] * j + \text{srow.x}[2] * k + \text{srow.x}[3] \\ y &= \text{srow.y}[0] * i + \text{srow.y}[1] * j + \text{srow.y}[2] * k + \text{srow.y}[3] \\ z &= \text{srow.z}[0] * i + \text{srow.z}[1] * j + \text{srow.z}[2] * k + \text{srow.z}[3] \end{aligned}$$

The srow.* vectors are in the NIFTI.1 header. Note that no use is made of pixdim[] in this method.

WHY 3 METHODS? ————— Method 1 is provided only for backwards compatibility. The intention is that Method 2 (qform.code > 0) represents the nominal voxel locations as reported by the scanner, or as rotated to some fiducial orientation and location. Method 3, if present (sform.code > 0), is to be used to give the location of the voxels in some standard space. The sform.code indicates which standard space is present. Both methods 2 and 3 can be present, and be useful in different contexts (method 2 for displaying the data on its original grid; method 3 for displaying it on a standard grid).

In this scheme, a dataset would originally be set up so that the Method 2 coordinates represent what the scanner reported. Later, a registration to some standard space can be computed and inserted in the header. Image display software can use either transform, depending on its purposes and needs.

In Method 2, the origin of coordinates would generally be whatever the scanner origin is; for example, in MRI, (0,0,0) is the center of the gradient coil.

In Method 3, the origin of coordinates would depend on the value of sform.code; for example, for the Talairach coordinate system, (0,0,0) corresponds to the Anterior Commissure.

QUATERNION REPRESENTATION OF ROTATION MATRIX (METHOD 2) —————

————— The orientation of the (x,y,z) axes relative to the (i,j,k) axes in 3D space is specified using a unit quaternion [a,b,c,d], where $a^2+b^2+c^2+d^2=1$. The (b,c,d) values are all that is needed, since we require that $a = \sqrt{1.0-(b^2+c^2+d^2)}$ be nonnegative. The (b,c,d) values are stored in the (quatern.b,quatern.c,quatern.d) fields.

The quaternion representation is chosen for its compactness in representing rotations. The (proper) 3x3 rotation matrix that corresponds to [a,b,c,d] is

$$\begin{bmatrix} a^2+b^2-b^2-c^2-d^2 & 2*b*c-2*a*d & 2*b*d+2*a*c \\ 2*b*c-2*a*d & a^2+c^2-b^2-d^2 & 2*c*d-2*a*b \\ 2*b*d+2*a*c & 2*c*d-2*a*b & a^2+d^2-c^2-b^2 \end{bmatrix} R = \begin{bmatrix} 2*b*c+2*a*d & a^2+c^2-b^2-d^2 & 2*c*d-2*a*b \\ 2*b*d+2*a*c & a^2+d^2-c^2-b^2 & \end{bmatrix}$$

$$\begin{bmatrix} R11 & R12 & R13 \end{bmatrix} = \begin{bmatrix} R21 & R22 & R23 \end{bmatrix} \begin{bmatrix} R31 & R32 & R33 \end{bmatrix}$$

If (p,q,r) is a unit 3-vector, then rotation of angle h about that direction is represented by the quaternion

$$[a,b,c,d] = [\cos(h/2), p*\sin(h/2), q*\sin(h/2), r*\sin(h/2)].$$

Requiring $a \geq 0$ is equivalent to requiring $-\pi \leq h \leq \pi$. (Note that [-a,-b,-c,-d] represents the same rotation as [a,b,c,d]; there are 2 quaternions that can be used to represent a given rotation matrix R.) To rotate a 3-vector (x,y,z) using quaternions, we compute the quaternion product

$$[0,x',y',z'] = [a,b,c,d] * [0,x,y,z] * [a,-b,-c,-d]$$

which is equivalent to the matrix-vector multiply

$$\begin{bmatrix} x' \\ y' \\ z' \end{bmatrix} = R \begin{bmatrix} x \\ y \\ z \end{bmatrix} \text{ (equivalence depends on } a^2+b^2+c^2+d^2=1)$$

Multiplication of 2 quaternions is defined by the following:

$$[a,b,c,d] = a*1 + b*I + c*J + d*K \text{ where } I*I = J*J = K*K = -1 \text{ (I,J,K are square roots of -1) } I*J = K \\ J*K = I \text{ K*I = J J*I = -K K*J = -I I*K = -J (not commutative!) For example } [a,b,0,0] * [0,0,0,1] = [0,0,-b,a] \text{ since this expands to } (a+b*I)*(K) = (a*K+b*I*K) = (a*K-b*J).$$

The above formula shows how to go from quaternion (b,c,d) to rotation matrix and direction cosines. Conversely, given R, we can compute the fields for the NIFTI-1 header by

$$a = 0.5 * \sqrt{1+R11+R22+R33} \text{ (not stored) } b = 0.25 * (R32-R23) / a \Rightarrow \text{quatern.b } c = 0.25 * (R13-R31) / a \Rightarrow \text{quatern.c } d = 0.25 * (R21-R12) / a \Rightarrow \text{quatern.d}$$

If $a=0$ (a 180 degree rotation), alternative formulas are needed. See the `nifti1.io.c` function `mat44.to.quatern()` for an implementation of the various cases in converting R to [a,b,c,d].

Note that R-transpose (= R-inverse) would lead to the quaternion [a,-b,-c,-d].

The choice to specify the `qoffset.x` (etc.) values in the final coordinate system is partly to make it easy to convert DICOM images to this format. The DICOM attribute "Image Position (Patient)" (0020,0032) stores the (Xd,Yd,Zd) coordinates of the center of the first voxel. Here, (Xd,Yd,Zd) refer to DICOM coordinates, and $Xd=-x$, $Yd=-y$, $Zd=z$, where (x,y,z) refers to the NIFTI coordinate system discussed above. (i.e., DICOM +Xd is Left, +Yd is Posterior, +Zd is Superior, whereas +x is Right, +y is Anterior, +z is Superior.) Thus, if the (0020,0032) DICOM attribute is extracted into (px,py,pz), then `qoffset.x = -px` `qoffset.y = -py` `qoffset.z = pz` is a reasonable setting when `qform.code=NIFTI.XFORM.SCANNER.ANAT`.

That is, DICOM's coordinate system is 180 degrees rotated about the z-axis from the neuroscience/NIFTI coordinate system. To transform between DICOM and NIFTI, you just have to negate the x- and y-coordinates.

The DICOM attribute (0020,0037) "Image Orientation (Patient)" gives the orientation of the x- and y-axes of the image data in terms of 2 3-vectors. The first vector is a unit vector along the x-axis, and the second is along the y-axis. If the (0020,0037) attribute is extracted into the value (xa,xb,xc,ya,yb,yc), then the first two columns of the R matrix would be [-xa -ya] [-xb -yb] [xc yc] The negations are because DICOM's x- and y-axes are reversed relative to NIFTI's. The third column of the R matrix gives the direction of displacement (relative to the subject) along the slice-wise direction. This orientation is not encoded in the DICOM standard in a simple way; DICOM is mostly concerned with 2D images. The third column of R will be either the cross-product of the first 2 columns or its negative. It is possible to infer the sign of the 3rd column by examining the coordinates in DICOM attribute (0020,0032) "Image Position (Patient)" for successive slices. However, this method occasionally fails for reasons that I (RW Cox) do not understand.

Value

A list containing the matrix xyz of the positions of the points specified in ijk.

See Also

[xyz2ijk Q2R R2Q](#)

Examples

```
L <- f.read.header(system.file("example-nifti.hdr",
package="AnalyzefMRI"))
ijk <- matrix(c(1,1,1,2,3,7),byrow=FALSE,nrow=3)
ijk2xyz(ijk=ijk,method=2,L)
```

magicfield

Get magicfield from the header of an image file

Description

Determine the type of a file : NIFIT .nii format, NIFTI .hdr/.img pair format, Analyze format.

Usage

```
magicfield(file)
```

Arguments

file character, filename of an image (or header) file

Value

A list containing the magic and dim fields.

Examples

```
magicfield(system.file("example-nifti.hdr", package="AnalyzeFMRI"))
```

mat34.to.TRSZ *Affine 4x4 (or 3x4) matrix to Translation, Rotation, Shear and Scale*

Description

Extract in that order Translation, Rotation, Shear and Scale from a 4x4 (or 3x4) affine matrix from a NIFTI header list (srow.x, srow.y, srow.z).

Usage

```
mat34.to.TRSZ(M)
```

Arguments

M the affine matrix

Value

A list containing Translation, Scale, Shear and Rotation.

See Also

[R2Q Q2R mat34.to.TZSR](#)

mat34.to.TZSR *Affine 4x4 (or 3x4) matrix to Translation, Scale, Shear and Rotation*

Description

Extract in that order Translation, Scale, Shear and Rotation from a 4x4 (or 3x4) affine matrix from a NIFTI header list (srow.x, srow.y, srow.z).

Usage

mat34.to.TZSR (M)

Arguments

M the affine matrix

Value

A list containing Translation, Scale, Shear and Rotation.

See Also

[R2Q Q2R mat34.to.TRSZ](#)

model.2.cov.func *Calculates covariance from Hartvig Model 2*

Description

Calculates covariance from Hartvig Model 2

Usage

model.2.cov.func (g, par)

Arguments

g The value of gamma
 par A vector of parameters from the N2G model

Value

The calculated covariance

Author(s)

J. L. Marchini

References

Hartvig, N. V. and Jensen, J. L (2000) Spatial Mixture Modelling of fMRI Data, Human Brain Mapping 11:233–248

`model.2.est.gamma` *Estimate gamma for Model 2 of Hartvig and Jensen (2000)*

Description

Estimate gamma for Model 2 of Hartvig and Jensen (2000)

Usage

```
model.2.est.gamma(cov, par)
```

Arguments

<code>cov</code>	An estimate of the spatial covariance
<code>par</code>	N2G model parameter estimates

Value

The estimate of gamma

Author(s)

J. L. Marchini

References

Hartvig, N. V. and Jensen, J. L (2000) Spatial Mixture Modelling of fMRI Data, Human Brain Mapping 11:233–248

`N2G` *Fits the N2G model*

Description

Fits the N2G model (1 Normal and 2 Gamma's mixture model) to a dataset using Maximum Likelihood.

Usage

```
N2G(data, par.start = c(4, 2, 4, 2, 0.9, 0.05))
```

Arguments

<code>data</code>	The dataset.
<code>par.start</code>	The starting values for the optimization to maximize the likelihood. The parameters of the model are ordered in the vector <code>par.start</code> in the following way (refer to the model below) <code>c(a, b, c, d, p1, p2)</code>

Details

The mixture model considered is a mixture of a standard normal distribution and two Gamma functions. This model is denoted N2G.

$$x \sim p1 * N(0, 1) + p2 * \text{Gamma}(a, b) + (1 - p1 - p2) * \text{-Gamma}(c, d)$$

Value

A list with components

<code>par</code>	The fitted parameter values.
<code>lims</code>	The upper and lower thresholds for the Normal component of the fitted model

Author(s)

J. L. Marchini

See Also

[N2G.Class.Probability](#), [N2G.Likelihood.Ratio](#), [N2G.Spatial.Mixture](#), [N2G.Density](#), [N2G.Likelihood](#), [N2G.Transform](#), [N2G.Fit](#), [N2G.Inverse](#), [N2G.Region](#)

Examples

```
par <- c(3, 2, 3, 2, .3, .4)
data <- c(rnorm(10000), rgamma(2000, 10, 1), -rgamma(1400, 10, 1))
hist(data, n = 100, freq = FALSE)

q <- N2G.Fit(data, par, maxit = 10000, method = "BFGS")
p <- seq(-50, 50, .1)
lines(p, N2G.Density(p, q), col = 2)
```

`N2G.Class.Probability`*Posterior Probabilities for N2G model*

Description

Calculates the Posterior Probability of data points being in each class given the parameters of the N2G model.

Usage

```
N2G.Class.Probability(data, par)
```

Arguments

<code>data</code>	The dataset (usually a vector)
<code>par</code>	The parameters of the model

Value

Returns the Posterior Probability of data points being in each class given the parameters of the N2G model.

Author(s)

J. L. Marchini

See Also

[N2G.Likelihood.Ratio](#), [N2G.Spatial.Mixture](#), [N2G.Density](#), [N2G.Likelihood](#), [N2G.Transform](#), [N2G.Fit](#), [N2G](#), [N2G.Inverse](#), [N2G.Region](#)

`N2G.Density`*Calculates the density function for the N2G model*

Description

Calculates the density function for the N2G model

Usage

```
N2G.Density(data, par)
```

Arguments

<code>data</code>	The dataset (usually a vector)
<code>par</code>	The parameters of the model.

Details

Calculates the density function for the N2G model

Value

Returns the density at each point of the datasets

Author(s)

J. L. Marchini

See Also

[N2G.Class.Probability](#), [N2G.Likelihood.Ratio](#), [N2G.Spatial.Mixture](#), [N2G.Likelihood](#), [N2G.Transform](#), [N2G.Fit](#), [N2G](#), [N2G.Inverse](#), [N2G.Region](#)

N2G.Fit

Optimization function for N2G model

Description

Function that carries out the likelihood optimization for the N2G model.

Usage

```
N2G.Fit(data, par.start, maxit, method)
```

Arguments

<code>data</code>	The dataset (usually a vector)
<code>par.start</code>	Starting values for the parameters
<code>maxit</code>	Maximum number of iterations
<code>method</code>	Optimization method (passed to <code>optim</code>)

Details

Numerical optimization of the N2G model likelihood.

Value

Returns the optimized model parameters.

Author(s)

J. L. Marchini

See Also

[N2G.Class.Probability](#), [N2G.Likelihood.Ratio](#), [N2G.Spatial.Mixture](#), [N2G.Likelihood](#), [N2G.Transform](#), [N2G.Density](#), [N2G](#), [N2G.Inverse](#), [N2G.Region](#)

N2G.Inverse

Transform parameters of N2G model back to their real domains

Description

Transform parameters of N2G model back to their real domains

Usage

N2G.Inverse(par)

Arguments

par Parameter vector

Details

Transform parameters of N2G model back to their real domains

Value

Returns the transformed parameters.

Author(s)

J. L. Marchini

See Also

[N2G.Class.Probability](#), [N2G.Likelihood.Ratio](#), [N2G.Spatial.Mixture](#), [N2G.Density](#), [N2G.Likelihood](#), [N2G.Transform](#), [N2G.Fit](#), [N2G](#), [N2G.Region](#)

N2G.Likelihood *Calculates the (negative) Likelihood of the N2G model*

Description

Calculates the (negative) Likelihood of the N2G model

Usage

```
N2G.Likelihood(inv.par, data)
```

Arguments

inv.par	A vector of transformed parameters for the N2G model
data	The dataset (usually a vector)

Details

Calculates the (negative) Likelihood of the N2G model

Value

Returns (negative) Likelihood at each point of the dataset.

Author(s)

J. L. Marchini

See Also

[N2G.Class.Probability](#), [N2G.Likelihood.Ratio](#), [N2G.Spatial.Mixture](#), [N2G.Density](#), [N2G.Transform](#), [N2G.Fit](#), [N2G](#), [N2G.Inverse](#), [N2G.Region](#)

N2G.Likelihood.Ratio
N2G Likelihood Ratio's

Description

Calculates the ratio of the likelihood that data came from the positive Gamma distribution (activation) to the likelihood that data came from the other two distributions (Normal and negative Gamma)

Usage

```
N2G.Likelihood.Ratio(data, par)
```

Arguments

data The dataset (usually a vector)
 par The parameter vector for the N2G model

Value

Returns the vector of likelihood ratio's

Author(s)

J. L. Marchini

See Also

[N2G.Class.Probability](#), [N2G.Spatial.Mixture](#), [N2G.Density](#), [N2G.Likelihood](#), [N2G.Transform](#), [N2G.Fit](#), [N2G](#), [N2G.Inverse](#), [N2G.Region](#)

N2G.Region

N2G Normal component interval

Description

Calculates the interval within which observations are classified as belonging to the Normal component of an N2G model.

Usage

`N2G.Region(par1)`

Arguments

par1 The parameters of the N2G model.

Value

A vector containing the upper and lower boundaries of the interval.

Author(s)

J. L. Marchini

See Also

[N2G.Class.Probability](#), [N2G.Likelihood.Ratio](#), [N2G.Spatial.Mixture](#), [N2G.Density](#), [N2G.Likelihood](#), [N2G.Transform](#), [N2G.Fit](#), [N2G](#), [N2G.Inverse](#)

 N2G.Spatial.Mixture

fMRI Spatial Mixture Modelling

Description

Fits the spatial mixture model of Hartvig and Jensen (2000)

Usage

```
N2G.Spatial.Mixture(data, par.start = c(4, 2, 4, 2, 0.9, 0.05), ksize, ktype = c("2D", "3D"), mask)
```

Arguments

data	The dataset (usually a vector)
par.start	Starting values for N2G model
ksize	Kernel size (see paper)
ktype	Format of kernel "2D" or "3D"
mask	Mask for dataset.

Value

p.map = a1, par = fitpar, lims = fitlims Returns a list with following components

p.map	Posterior Probability Map of activation
par	Fitted parameters of the underlying N2G model
lims	Normal component interval for fitted model

Author(s)

J. L. Marchini

References

Hartvig and Jensen (2000) Spatial Mixture Modelling of fMRI Data

See Also

[N2G.Class.Probability](#), [N2G.Likelihood.Ratio](#), [N2G.Density](#), [N2G.Likelihood](#), [N2G.Transform](#), [N2G.Fit](#), [N2G](#), [N2G.Inverse](#), [N2G.Region](#)

Examples

```

## simulate image
d <- c(100, 100, 1)
y <- array(0, dim = d)
m <- y
m[, , ] <- 1

z.init <- 2 * m
z.init[20:40, 20:40, 1] <- 1
z.init[50:70, 50:70, 1] <- 3

y[z.init == 1] <- rgamma(sum(z.init == 1), 4, 1)
y[z.init == 2] <- rnorm(sum(z.init == 2))
y[z.init == 3] <- rgamma(sum(z.init == 3), 4, 1)

mask <- 1 * (y < 1000)

## fit spatial mixture model
ans <- N2G.Spatial.Mixture(y, par.start = c(4, 2, 4, 2, 0.9, 0.05), ksize = 3, ktype = "2D",

## plot original image, standard mixture model estimate and spatial mixture
## model estimate

par(mfrow = c(1, 3))
image(y[, , 1])
image(y[, , 1] > ans$lims[1]) ## this line plots the results of a Non-Spatial Mixture Model
image(ans$p.map[, , 1] > 0.5) ## this line plots the results of the Spatial Mixture Model

```

N2G.Transform

Transform parameters of N2G model so as to lie on the real line.

Description

Transform parameters of N2G model so as to lie on the real line

Usage

```
N2G.Transform(par)
```

Arguments

par Parameter vector for N2G model.

Details

Transformation required for optimization.

Value

Returns the transformed parameters.

Author(s)

J. L. Marchini

See Also

[N2G.Class.Probability](#), [N2G.Likelihood.Ratio](#), [N2G.Spatial.Mixture](#), [N2G.Density](#), [N2G.Likelihood](#), [N2G.Fit](#), [N2G](#), [N2G.Inverse](#), [N2G.Region](#)

nifti.quatern.to.mat44

Quaternion (etc..) to affine 4x4 matrix

Description

Generate a 4x4 affine matrix from a NIFIT header list.

Usage

nifti.quatern.to.mat44(L)

Arguments

L a NIFIT header list

Value

The 4x4 affine matrix.

See Also

[R2Q Q2R](#)

`NonLinearSmoothArray`*Non-linear spatial smmoothing of 3D and 4D arrays.*

Description

Smooths the values in an array spatially using a weighting kernel that doesn't smooth across boundaries.

Usage

```
NonLinearSmoothArray(x, voxdim=c(1, 1, 1), radius=2, sm=3, mask=NULL)
```

Arguments

<code>x</code>	The array to be smoothed.
<code>voxdim</code>	The voxel dimensions of the array.
<code>radius</code>	The radius of the spatial smoothing
<code>sm</code>	The standard deviation of the Gaussian smoothing kernel.
<code>mask</code>	Optional mask for smoothing.

Details

For a 3D array the smoothed values are obtained through a weighted sum of the surrounding voxel values within the specified radius. The weights are calculated using a Gaussian kernel function applied to the differences between the voxel and its surrounding voxels. In this way the smoothing is anisotropic.

For a 4D array the first 3 dimensions represent space and the fourth represents time. Therefore, each spatial location contains a time series of values. These time series are smoothed spatially in an anisotropic fashion. The sum of squared differences between each pair of time series are used to define the smoothing weights.

Value

The smoothed array is returned.

Author(s)

J. L. Marchini

See Also

[GaussSmoothArray](#)

Examples

```

#3D array
d<-rep(10,3)
a<-array(3,dim=d)
a[,5:10,5:10]<-7
a<-a+array(rnorm(n=1000,sd=1),dim=d)

h<-NonLinearSmoothArray(a,voxdim=c(1,1,1),radius=2,sm=3)

par(mfrow=c(2,2))
image(a[1,,],zlim=c(-1,12));title("Before smoothing")
image(h[1,,],zlim=c(-1,12));title("After smoothing")
persp(a[1,,],zlim=c(-1,12))
persp(h[1,,],zlim=c(-1,12))

#4D array
d<-c(10,10,10,20)
a<-array(1,dim=d)
a[, , 6:10, ]<-2
a<-a+array(rnorm(20000,sd=.1),dim=d)

h<-NonLinearSmoothArray(a,voxdim=c(1,1,1),radius=2,sm=3)

par(mfrow=c(2,2),mar=c(0,0,0,0))
for(i in 1:10){
  for(j in 10:1){
    plot(a[1,i,j,],type="l",ylim=c(0,3),axes=FALSE);box()
    lines(h[1,i,j,],col=2)
  }}

```

Q2R

Quaternion to rotation

Description

Generate a rotation matrix from a quaternion.

Usage

```
Q2R(Q, qfac)
```

Arguments

Q quaternion vector
qfac qfac nifti field. It is pixdim[1]

Value

The rotation.

See Also

[R2Q](#)

R2Q

Rotation to quaternion

Description

Convert from rotation matrix to quaternion form.

Usage

R2Q (R)

Arguments

R Rotation matrix

Value

The quaternion.

See Also

[Q2R](#)

reduction

reduction

Description

This function reduces the data in the row or col dimension.

Usage

reduction(X, row.red=TRUE)

Arguments

X a matrix of size $t_m \times v_m$ which contains the functionnal images
row.red Logical. Reduces the columns or the rows

Value

Xred the reduced matrix

See Also

[centering](#)

Examples

```
# TODO!!
# Xcr <- reduction(Xcentred, row.red=TRUE) $Xred
```

Sim.3D.GammaRF *Simulate Gamma distributed Random Field*

Description

Simulates a Gamma distributed random field by simulating a Gaussian Random Field and transforming it to be Gamma distributed.

Usage

```
Sim.3D.GammaRF(d, voxdim, sigma, ksize, mask, shape, rate)
```

Arguments

d	A vector specifying the dimensions of a 3D or 4D array.
voxdim	The dimensions of each voxel.
sigma	The 3D covariance matrix of the field.
ksize	The size (in voxels) of the kernel with which to filter the independent field.
mask	A 3D mask for the field.
shape	The shape parameter of the Gamma distribution.
rate	The rate parameter of the Gamma distribution.

Value

A 3D array containing the simulated field

Author(s)

J. L. Marchini

Examples

```
d <- c(64, 64, 21)
FWHM <- 9
sigma <- diag(FWHM^2, 3) / (8 * log(2))
voxdim <- c(2, 2, 4)
m <- array(1, dim = d)

a <- Sim.3D.GammaRF(d = d, voxdim = voxdim, sigma = sigma,
                   ksize = 9, mask = m, shape = 6, rate = 1)
```

 Sim.3D.GRF

Simulate a GRF

Description

Simulates a Gaussian Random Field with specified dimensions and covariance structure.

Usage

```
Sim.3D.GRF(d, voxdim, sigma, ksize, mask = NULL, type = c("field", "max"))
```

Arguments

d	A vector specifying the dimensions of a 3D or 4D array.
voxdim	The dimensions of each voxel.
sigma	The 3D covariance matrix of the field.
ksize	The size (in voxels) of the kernel with which to filter the independent field.
mask	A 3D mask for the field.
type	If type == "field" then the simulated field together with the maximum of the field is returned. If type == "max" then the maximum of the field is returned.

Details

The function works by simulating a Gaussian r.v at each voxel location and then smoothing the field with a discrete filter to obtain a field with the desired covariance structure.

Value

mat	Contains the simulated field if type == "field", else NULL
max	The maximum value of the simulated field.

Author(s)

J. L. Marchini

See Also

[GaussSmoothArray](#), [GaussSmoothKernel](#)

Examples

```
d <- c(64, 64, 21)
FWHM <- 9
sigma <- diag(FWHM^2, 3) / (8 * log(2))
voxdim <- c(2, 2, 4)
msk <- array(1, dim = d)

field <- Sim.3D.GRF(d = d, voxdim = voxdim, sigma = sigma, ksize = 9, mask = msk, type = "ma
```

SmoothEst

Estimate the variance-covariance matrix of a Gaussian random field

Description

Estimate the variance-covariance matrix of a Gaussian random field

Usage

```
SmoothEst(mat, mask, voxdim, method = "Forman")
```

Arguments

mat	3D array that is the Gaussian Random Field.
mask	3D mask array.
voxdim	Vector of length 3 containing the voxel dimensions.
method	The estimator to use. method = "Forman" (the default) uses the estimator proposed in [1]. method = "Friston" uses the estimator proposed in [2, 3], but tis can be biased when the amount of smoothing is small compared to the size of each voxel (see [1] for more details and example below)

Details

Calculates the varaince-covariance matrix using the variance covariance matrix of partial derivatives.

Value

A (3x3) diagonal matrix.

Author(s)

J. L. Marchini

References

- [1] Stephen D. Forman et al. (1995) Improved assessment of significant activation in functional magnetic resonance imaging (fMRI): Use of a cluster-size threshold. *Magnetic Resonance in Medicine*, 33:636-647.
- [2] Karl J. Friston et al. (1991) Comparing functional (PET) images: the assessment of significant change. *J. Cereb. Blood Flow Metab.* 11:690-699.
- [3] Stefan J. Kiebel et al. (1999) Robust smoothness estimation in statistical parametric maps using standardized residuals from the general linear model. *NeuroImage*, 10:756-766.

Examples

```
#####
## EXAMPLE 1 ##
#####
## example that illustrates the bias of the Friston
## method when smoothing is small compared to voxel size
## NB. The presence of bias becomes clearer if the
##     simulations below are run about 100 times and
##     the results averaged

ksize <- 13
d <- c(64, 64, 64)
voxdim <- c(1, 1, 1)
FWHM <- 2 ## using a small value of FWHM (=2) compared to voxel size (=1)
sigma <- diag(FWHM^2, 3) / (8 * log(2))
mask <- array(1, dim = d)
num.vox <- sum(mask)

grf <- Sim.3D.GRF(d = d, voxdim = voxdim, sigma = sigma, ksize = ksize, mask = mask, type =
sigma
SmoothEst(grf, mask, voxdim, method = "Friston")
SmoothEst(grf, mask, voxdim, method = "Forman") ## compared to sigma
##the Forman estimator is better (on average) than the Friston estimator

#####
## EXAMPLE 2 ##
#####
## increasing the amount of smoothing decreases the bias of the Friston estimator

ksize <- 13
d <- c(64, 64, 64)
voxdim <- c(1, 1, 1)
FWHM <- 5 ## using a large value of FWHM (=5) compared to voxel size (=1)
sigma <- diag(FWHM^2, 3) / (8 * log(2))
mask <- array(1, dim = d)
num.vox <- sum(mask)

grf <- Sim.3D.GRF(d = d, voxdim = voxdim, sigma = sigma, ksize = ksize, mask = mask, type =
```

```
SmoothEst(grf, mask, voxdim, method = "Friston")
SmoothEst(grf, mask, voxdim, method = "Forman")
sigma
```

st2xyzt

st2xyzt

Description

Encode space and time dimensions fields into the one byte xyzt.units field of a NIFTI header file.

Usage

```
st2xyzt(space, time)
```

Arguments

space	space field of a NIFTI file
time	time field of a NIFTI file

Value

A list containing xyzt.units field.

See Also

[xyzt2st](#)

Examples

```
xyzt.units <- f.read.header(system.file("example-nifti.hdr", package="AnalyzeFMRI"))$xyzt.un
mylist <- xyzt2st(xyzt.units)
st2xyzt(mylist$space, mylist$time)
```

threeDto4D

threeDto4D

Description

To read tm fonctionnal images in ANALYZE or NIFTI format, and concatenate them to obtain one 4D image file in Analyze (hdr/img pair) or Nifti format (hdr/img pair or single nii) which is written on disk.

Usage

```
threeDto4D(outputfile, path.in=NULL, prefix=NULL, regexp=NULL, times=NULL, list.of.in.fi
```

Arguments

<code>outputfile</code>	character. Name of the outputfile without extension
<code>path.in</code>	character with the path to the directory containing the image files
<code>prefix</code>	character. common prefix to each file
<code>regex</code>	character. Regular expression to get all the files
<code>times</code>	vector. numbers of the image files to retrieve
<code>list.of.in.files</code>	names of img files to concatenate (with full path)
<code>path.out</code>	where to write the output hdr/img pair files. Will be taken as path.in if not provided.
<code>is.nii.pair</code>	logical. Should we write a single nii NIFTI file or a hdr/img NIFTI pair file
<code>hdr.number</code>	Number of the original 3D Analyze or NIFTI image file from which to take the header that should serve as the final header of the newly 4D created image file

Value

None.

See Also

[twoDto4D](#) [fourDto2D](#)

Examples

```
# path.fonc <- "/network/home/lafayep/Stage/Data/map284/functional/MondrianApril2007/preproc"
# threeDto4D("essai", path.in=path.fonc, prefix="sul801_", regex="?????.img", times=1:120)
```

Threshold.Bonferroni

Calculates Bonferroni Threshold

Description

Calculate the Bonferroni threshold for n iid tests that results in an overall p-value of `p.val`. The tests can be distributed as Normal, t or F.

Usage

```
Threshold.Bonferroni(p.val, n, type = c("Normal", "t", "F"), df1 = NULL, df2 = NULL)
```

Arguments

<code>p.val</code>	The required overall p-value.
<code>n</code>	The number of tests.
<code>type</code>	The distribution of the tests. One of "Normal", "t" or "F"
<code>df1</code>	The degrees of freedom of the t-distribution or the first degrees of freedom parameter for the F distribution.
<code>df2</code>	The second degrees of freedom parameter for the F distribution.

Value

Returns the Bonferroni threshold.

Examples

```
Threshold.Bonferroni(0.05, 1000)
Threshold.Bonferroni(0.05, 1000, type = c("t"), df1 = 20)
Threshold.Bonferroni(0.05, 1000, type = c("F"), df1 = 3, df2 = 100)
```

`Threshold.FDR` *False Discovery Rate (FDR) Threshold*

Description

Calculates the False Discovery Rate (FDR) threshold for a given vector of statistic values..

Usage

```
Threshold.FDR(x, q, cV.type = 2, type = c("Normal", "t", "F"), df1 = NULL, df2 = NU
```

Arguments

<code>x</code>	A vector of p-values.
<code>q</code>	The desired False Discovery Rate threshold.
<code>cV.type</code>	A flag that specifies the assumptions about the joint distribution of p-values. Choose <code>cV.type = 2</code> for fMRI data (see Genovese et al (2001))
<code>type</code>	The distribution of the statistic values. Either "Normal", "t" or "F".
<code>df1</code>	The degrees of freedom of the t-distribution or the first degrees of freedom parameter for the F distribution.
<code>df2</code>	The second degrees of freedom parameter for the F distribution.

Value

Returns the FDR threshold.

Author(s)

J. L. Marchini

References

Genovese et al. (2001) Thresholding of Statistical Maps in Functional NeuroImaging Using the False Discovery Rate.

Examples

```
x <- c(rnorm(1000), rnorm(100, mean = 3))
Threshold.FDR(x = x, q = 0.20, cV.type = 2)
```

Threshold.RF *Random Field Theory Thresholds.*

Description

Calculates the Random Field theory threshold to give that results in a specified p-value.

Usage

```
Threshold.RF(p.val, sigma, voxdim = c(1, 1, 1), num.vox, type = c("Normal", "t"), c
```

Arguments

p.val	The required p-value.
sigma	The 3D covariance matrix of the random field.
voxdim	The dimesnions of a voxel.
num.vox	The number of voxels that constitute the random field.
type	The type of random field, "Normal" or "t".
df	The degrees of the t distributed field.

Details

Calculates the threshold that produces an expected Euler characteristic equal to the required p-value.

Value

Returns the Random Field threshold.

Author(s)

J. L. Marchini

See Also[EC.3D](#)**Examples**

```
a <- Threshold.RF(p.val = 0.05, sigma = diag(1, 3), voxdim = c(1, 1, 1), num.vox = 10000)
EC.3D(a, sigma = diag(1, 3), voxdim = c(1, 1, 1), num.vox = 10000)
```

`twoDto4D`*twoDto4D*

Description

This function transform a 2D matrix of size $t_m \times v_m$ containing images in each row into a 4D array image.

Usage

```
twoDto4D(x.2d, dim)
```

Arguments

<code>x.2d</code>	a 2D matrix to be transformed
<code>dim</code>	vector of length 4 containing the dimensions of the array. <code>dim[1:3]</code> are the space dimensions. <code>dim[4]</code> is the time dimension

Value

<code>volume.4d</code>	a 4D array image
------------------------	------------------

See Also[threeDto4D](#) [fourDto2D](#)

 xyz2ijk

 xyz2ijk

Description

This function maps from some real world (x,y,z) positions in space into data coordinates (e.g. column i, row j, slice k). These original positions could relate to Talairach-Tournoux (T&T) space, MNI space, or patient-based scanner coordinates.

Usage

```
xyz2ijk(xyz=c(1,1,1),method=2,L)
```

Arguments

xyz	matrix. Each column of xyz should contain a voxel real world index coordinates (x,y,z) to be mapped to its (i,j,k) voxel index coordinates in the dataset
method	1 (qform.code=sform.code=0), 2 (qform.code>0, rigid transformation) or 3 (sform.code>0, affine transformation).
L	header list of a NIFTI file

Details

The NIFTI format allows storage on disk to be in either a left- or right-handed coordinate system. However, the format includes an implicit spatial transformation into a RIGHT-HANDED coordinate system. This transform maps from data coordinates (e.g. column i, row j, slice k), into some real world (x,y,z) positions in space. These positions could relate to Talairach-Tournoux (T&T) space, MNI space, or patient-based scanner coordinates. For T&T, and MNI coordinates, x increases from left to right, y increases from posterior to anterior, and z increases in the inferior to superior direction. Directions in the scanner coordinate system are similar. MRI data is usually exported as DICOM format, which encodes the positions and orientations of the slices. When data are converted from DICOM to NIFTI-1 format, the relevant information can be determined from the Pixel Spacing, Image Orientation (Patient) and Image Position (Patient) fields of the DICOM files. NIFTI-1 also allows the space of one image to be mapped to that of another (via a rigid or affine transform). This is to enable on-the-fly resampling of registered images. This would allow intra-subject images, collected with lots of different orientations or resolutions, to be treated as if they are all in register.

Neurological and radiological conventions only relate to visualization of axial images. They are unrelated to how the data are stored on disk, or even how the real-world coordinates are represented. It is more appropriate to consider whether the real-world coordinate system is left- or right-handed (see below). Talairach and Tournoux use a right-handed system, whereas the storage convention of ANALYZE files is usually considered as left-handed. These coordinate systems are mirror images of each other (if you are a psychologist, try explaining why mirror images appear to be left-right flipped, rather than flipped up-down, or back-front). Transforming between left- and right-handed coordinate systems involves flipping, and can not be done by rotations alone.

x=pouce, y=index, z=majeur de la main gauche (resp. droite) pour les droitiers (resp. gauchers)

Volume orientation is given by a transformation that maps voxel indices (i,j,k) to spatial coordinates (x,y,z), typically anatomical coordinates assigned by the scanner. This transformation ("Method 2" in the nifti1.h documentation) is generated using the voxel dimensions, a quaternion encoding a rotation matrix, and a 3D shift, all stored in the NIFTI-1 header; details can be found in the nifti1.h comments. The NIFTI-1 header also provides for a general affine transformation, separate from that described by Method 2. This transformation ("Method 3") also maps voxel indices (i,j,k) to (x,y,z), which in this case are typically coordinates in a standard space such as the Talairach space. The elements of this transformation matrix are stored in the NIFTI-1 header. For example, the Method 2 transformation can be constructed from the attributes from a set of DICOM files; the Method 3 transform can be computed offline and inserted into the header later. The exact "meaning" of the coordinates given by the Method 2 and Method 3 transformations is recorded in header fields qform.code and sform.code, respectively. Code values can indicate if the (x,y,z) axes are Anatomical coordinates from the scanner (e.g., the DICOM header) Aligned to some anatomical "truth" or standard Aligned and warped to Talairach-Tournoux coordinates Aligned and warped to MNI-152 coordinates

It is possible that neither transformation is specified (i.e., qform.code=sform.code=0), in which case we are left with the voxel size in pixdim[], and no orientation is given or assumed. This use ("Method 1") is discouraged.

The basic idea behind having two coordinate systems is to allow the image to store information about (1) the scanner coordinate system used in the acquisition of the volume (in the qform) and (2) the relationship to a standard coordinate system - e.g. MNI coordinates (in the sform). The qform allows orientation information to be kept for alignment purposes without losing volumetric information, since the qform only stores a rigid-body transformation which preserves volume. On the other hand, the sform stores a general affine transformation which can map the image coordinates into a standard coordinate system, like Talairach or MNI, without the need to resample the image. By having both coordinate systems, it is possible to keep the original data (without resampling), along with information on how it was acquired (qform) and how it relates to other images via a standard space (sform). This ability is advantageous for many analysis pipelines, and has previously required storing additional files along with the image files. By using NIFTI-1 this extra information can be kept in the image files themselves. Note: the qform and sform also store information on whether the coordinate system is left-handed or right-handed (see Q15) and so when both are set they must be consistent, otherwise the handedness of the coordinate system (often used to distinguish left-right order) is unknown and the results of applying operations to such an image are unspecified.

There are 3 different methods by which continuous coordinates can be attached to voxels. The discussion below emphasizes 3D volumes, and the continuous coordinates are referred to as (x,y,z). The voxel index coordinates (i.e., the array indexes) are referred to as (i,j,k), with valid ranges: $i = 0 \dots \text{dim}[1]-1$ $j = 0 \dots \text{dim}[2]-1$ (if $\text{dim}[0] \geq 2$) $k = 0 \dots \text{dim}[3]-1$ (if $\text{dim}[0] \geq 3$) The (x,y,z) coordinates refer to the CENTER of a voxel. In methods 2 and 3, the (x,y,z) axes refer to a subject-based coordinate system, with +x = Right +y = Anterior +z = Superior. This is a right-handed coordinate system. However, the exact direction these axes point with respect to the subject depends on qform.code (Method 2) and sform.code (Method 3).

N.B.: The i index varies most rapidly, j index next, k index slowest. Thus, voxel (i,j,k) is stored starting at location $(i + j*\text{dim}[1] + k*\text{dim}[1]*\text{dim}[2]) * (\text{bitpix}/8)$ into the dataset array.

N.B.: The ANALYZE 7.5 coordinate system is +x = Left +y = Anterior +z = Superior which is a left-handed coordinate system. This backwardness is too difficult to tolerate, so this NIFTI-1 standard specifies the coordinate order which is most common in functional neuroimaging.

N.B.: The 3 methods below all give the locations of the voxel centers in the (x,y,z) coordinate

system. In many cases, programs will wish to display image data on some other grid. In such a case, the program will need to convert its desired (x,y,z) values into (i,j,k) values in order to extract (or interpolate) the image data. This operation would be done with the inverse transformation to those described below.

N.B.: Method 2 uses a factor 'qfac' which is either -1 or 1; qfac is stored in the otherwise unused pixdim[0]. If pixdim[0]=0.0 (which should not occur), we take qfac=1. Of course, pixdim[0] is only used when reading a NIFTI-1 header, not when reading an ANALYZE 7.5 header.

N.B.: The units of (x,y,z) can be specified using the xyzt.units field.

METHOD 1 (the "old" way, used only when qform.code = 0): _____
 _____ The coordinate mapping from (i,j,k) to (x,y,z) is the ANALYZE 7.5 way. This is a simple scaling relationship:

$$x = \text{pixdim}[1] * i \quad y = \text{pixdim}[2] * j \quad z = \text{pixdim}[3] * k$$

No particular spatial orientation is attached to these (x,y,z) coordinates. (NIFTI-1 does not have the ANALYZE 7.5 orient field, which is not general and is often not set properly.) This method is not recommended, and is present mainly for compatibility with ANALYZE 7.5 files.

METHOD 2 (used when qform.code > 0, which should be the "normal" case): _____
 _____ The (x,y,z) coordinates are given by the pixdim[] scales, a rotation matrix, and a shift. This method is intended to represent "scanner-anatomical" coordinates, which are often embedded in the image header (e.g., DICOM fields (0020,0032), (0020,0037), (0028,0030), and (0018,0050)), and represent the nominal orientation and location of the data. This method can also be used to represent "aligned" coordinates, which would typically result from some post-acquisition alignment of the volume to a standard orientation (e.g., the same subject on another day, or a rigid rotation to true anatomical orientation from the tilted position of the subject in the scanner). The formula for (x,y,z) in terms of header parameters and (i,j,k) is:

$$\begin{bmatrix} x \\ y \\ z \end{bmatrix} = \begin{bmatrix} R11 & R12 & R13 \\ R21 & R22 & R23 \\ R31 & R32 & R33 \end{bmatrix} \begin{bmatrix} \text{pixdim}[1] * i \\ \text{pixdim}[2] * j \\ \text{qfac} * \text{pixdim}[3] * k \end{bmatrix} + \begin{bmatrix} \text{qoffset.x} \\ \text{qoffset.y} \\ \text{qoffset.z} \end{bmatrix}$$

The qoffset.* shifts are in the NIFTI-1 header. Note that the center of the (i,j,k)=(0,0,0) voxel (first value in the dataset array) is just (x,y,z)=(qoffset.x,qoffset.y,qoffset.z).

The rotation matrix R is calculated from the quatern.* parameters. This calculation is described below.

The scaling factor qfac is either 1 or -1. The rotation matrix R defined by the quaternion parameters is "proper" (has determinant 1). This may not fit the needs of the data; for example, if the image grid is i increases from Left-to-Right j increases from Anterior-to-Posterior k increases from Inferior-to-Superior Then (i,j,k) is a left-handed triple. In this example, if qfac=1, the R matrix would have to be

$$\begin{bmatrix} 1 & 0 & 0 \\ 0 & -1 & 0 \\ 0 & 0 & 1 \end{bmatrix} \text{ which is "improper" (determinant} = -1). \begin{bmatrix} 0 & 0 & 1 \\ 0 & -1 & 0 \\ 1 & 0 & 0 \end{bmatrix}$$

If we set qfac=-1, then the R matrix would be

$$\begin{bmatrix} 1 & 0 & 0 \\ 0 & -1 & 0 \\ 0 & 0 & -1 \end{bmatrix} \text{ which is proper. } \begin{bmatrix} 0 & 0 & -1 \\ 0 & -1 & 0 \\ 1 & 0 & 0 \end{bmatrix}$$

This R matrix is represented by quaternion [a,b,c,d] = [0,1,0,0] (which encodes a 180 degree rotation about the x-axis).

METHOD 3 (used when sform.code > 0): _____ The (x,y,z) coordinates are given by a general affine transformation of the (i,j,k) indexes:

$$\begin{aligned} x &= \text{srow.x}[0] * i + \text{srow.x}[1] * j + \text{srow.x}[2] * k + \text{srow.x}[3] \\ y &= \text{srow.y}[0] * i + \text{srow.y}[1] * j + \text{srow.y}[2] * k + \text{srow.y}[3] \\ z &= \text{srow.z}[0] * i + \text{srow.z}[1] * j + \text{srow.z}[2] * k + \text{srow.z}[3] \end{aligned}$$

The srow.* vectors are in the NIFTI.1 header. Note that no use is made of pixdim[] in this method.

WHY 3 METHODS? ————— Method 1 is provided only for backwards compatibility. The intention is that Method 2 (qform.code > 0) represents the nominal voxel locations as reported by the scanner, or as rotated to some fiducial orientation and location. Method 3, if present (sform.code > 0), is to be used to give the location of the voxels in some standard space. The sform.code indicates which standard space is present. Both methods 2 and 3 can be present, and be useful in different contexts (method 2 for displaying the data on its original grid; method 3 for displaying it on a standard grid).

In this scheme, a dataset would originally be set up so that the Method 2 coordinates represent what the scanner reported. Later, a registration to some standard space can be computed and inserted in the header. Image display software can use either transform, depending on its purposes and needs.

In Method 2, the origin of coordinates would generally be whatever the scanner origin is; for example, in MRI, (0,0,0) is the center of the gradient coil.

In Method 3, the origin of coordinates would depend on the value of sform.code; for example, for the Talairach coordinate system, (0,0,0) corresponds to the Anterior Commissure.

QUATERNION REPRESENTATION OF ROTATION MATRIX (METHOD 2) —————

————— The orientation of the (x,y,z) axes relative to the (i,j,k) axes in 3D space is specified using a unit quaternion [a,b,c,d], where $a^2+b^2+c^2+d^2=1$. The (b,c,d) values are all that is needed, since we require that $a = \sqrt{1.0-(b^2+c^2+d^2)}$ be nonnegative. The (b,c,d) values are stored in the (quatern.b,quatern.c,quatern.d) fields.

The quaternion representation is chosen for its compactness in representing rotations. The (proper) 3x3 rotation matrix that corresponds to [a,b,c,d] is

$$\begin{bmatrix} a^2+b^2-b^2-c^2-d^2 & 2*b*c-2*a*d & 2*b*d+2*a*c \\ 2*b*c-2*a*d & a^2+c^2-b^2-d^2 & 2*c*d-2*a*b \\ 2*b*d+2*a*c & 2*c*d-2*a*b & a^2+d^2-c^2-b^2 \end{bmatrix} R = \begin{bmatrix} 2*b*c+2*a*d & a^2+c^2-b^2-d^2 & 2*c*d-2*a*b \\ 2*b*d-2*a*c & 2*c*d+2*a*b & a^2+d^2-c^2-b^2 \end{bmatrix}$$

$$\begin{bmatrix} R11 & R12 & R13 \end{bmatrix} = \begin{bmatrix} R21 & R22 & R23 \end{bmatrix} \begin{bmatrix} R31 & R32 & R33 \end{bmatrix}$$

If (p,q,r) is a unit 3-vector, then rotation of angle h about that direction is represented by the quaternion

$$[a,b,c,d] = [\cos(h/2), p*\sin(h/2), q*\sin(h/2), r*\sin(h/2)].$$

Requiring $a \geq 0$ is equivalent to requiring $-\pi \leq h \leq \pi$. (Note that [-a,-b,-c,-d] represents the same rotation as [a,b,c,d]; there are 2 quaternions that can be used to represent a given rotation matrix R.) To rotate a 3-vector (x,y,z) using quaternions, we compute the quaternion product

$$[0,x',y',z'] = [a,b,c,d] * [0,x,y,z] * [a,-b,-c,-d]$$

which is equivalent to the matrix-vector multiply

$$\begin{bmatrix} x' \\ y' \\ z' \end{bmatrix} = R \begin{bmatrix} x \\ y \\ z \end{bmatrix} \text{ (equivalence depends on } a^2+b^2+c^2+d^2=1)$$

Multiplication of 2 quaternions is defined by the following:

$$[a,b,c,d] = a*1 + b*I + c*J + d*K \text{ where } I*I = J*J = K*K = -1 \text{ (I,J,K are square roots of -1) } I*J = K \\ J*K = I \text{ K*I = J J*I = -K K*J = -I I*K = -J (not commutative!) For example } [a,b,0,0] * [0,0,0,1] = [0,0,-b,a] \text{ since this expands to } (a+b*I)*(K) = (a*K+b*I*K) = (a*K-b*J).$$

The above formula shows how to go from quaternion (b,c,d) to rotation matrix and direction cosines. Conversely, given R, we can compute the fields for the NIFTI-1 header by

$$a = 0.5 * \sqrt{1+R11+R22+R33} \text{ (not stored) } b = 0.25 * (R32-R23) / a \Rightarrow \text{quatern.b} \\ c = 0.25 * (R13-R31) / a \Rightarrow \text{quatern.c} \\ d = 0.25 * (R21-R12) / a \Rightarrow \text{quatern.d}$$

If $a=0$ (a 180 degree rotation), alternative formulas are needed. See the `nifti1.io.c` function `mat44.to.quatern()` for an implementation of the various cases in converting R to [a,b,c,d].

Note that R-transpose (= R-inverse) would lead to the quaternion [a,-b,-c,-d].

The choice to specify the `qoffset.x` (etc.) values in the final coordinate system is partly to make it easy to convert DICOM images to this format. The DICOM attribute "Image Position (Patient)" (0020,0032) stores the (Xd,Yd,Zd) coordinates of the center of the first voxel. Here, (Xd,Yd,Zd) refer to DICOM coordinates, and $Xd=-x$, $Yd=-y$, $Zd=z$, where (x,y,z) refers to the NIFTI coordinate system discussed above. (i.e., DICOM +Xd is Left, +Yd is Posterior, +Zd is Superior, whereas +x is Right, +y is Anterior, +z is Superior.) Thus, if the (0020,0032) DICOM attribute is extracted into (px,py,pz), then `qoffset.x = -px` `qoffset.y = -py` `qoffset.z = pz` is a reasonable setting when `form.code=NIFTI.XFORM.SCANNER.ANAT`.

That is, DICOM's coordinate system is 180 degrees rotated about the z-axis from the neuroscience/NIFTI coordinate system. To transform between DICOM and NIFTI, you just have to negate the x- and y-coordinates.

The DICOM attribute (0020,0037) "Image Orientation (Patient)" gives the orientation of the x- and y-axes of the image data in terms of 2 3-vectors. The first vector is a unit vector along the x-axis, and the second is along the y-axis. If the (0020,0037) attribute is extracted into the value (xa,xb,xc,ya,yb,yc), then the first two columns of the R matrix would be [-xa -ya] [-xb -yb] [xc yc] The negations are because DICOM's x- and y-axes are reversed relative to NIFTI's. The third column of the R matrix gives the direction of displacement (relative to the subject) along the slice-wise direction. This orientation is not encoded in the DICOM standard in a simple way; DICOM is mostly concerned with 2D images. The third column of R will be either the cross-product of the first 2 columns or its negative. It is possible to infer the sign of the 3rd column by examining the coordinates in DICOM attribute (0020,0032) "Image Position (Patient)" for successive slices. However, this method occasionally fails for reasons that I (RW Cox) do not understand.

Value

A list containing the matrix xyz of the positions of the points specified in ijk.

See Also

[ijk2xyz Q2R R2Q](#)

Examples

```
L <- f.read.header(system.file("example-nifti.hdr",
package="AnalyzeFMRI"))
xyz <- matrix(c(1,1,1,2,3,7),byrow=FALSE,nrow=3)
xyz2ijk(xyz=xyz,method=2,L)
```

xyzt2st

xyzt2st

Description

Extract space and time dimensions fields from the one byte `xyzt.units` field of a NIFTI header file.

Usage

```
xyzt2st(xyzt.units)
```

Arguments

```
xyzt.units    xyzt.units field of a NIFTI header file
```

Value

A list containing space and time fields.

See Also

[st2xyzt](#)

Examples

```
xyzt.units <- f.read.header(system.file("example-nifti.hdr", package="AnalyzeFMRI"))$xyzt.un  
xyzt2st(xyzt.units)
```

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